



# Modular J-PET applications in medical and particle physics

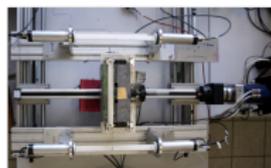
**S. Sharma**

on behalf of the JPET collaboration

- ① Jagiellonian **P**ositron **E**mission **T**omograph
- ② Studies with Positronium decays
- ③ Modular **J-PET** : *Portable tomograph* (AFOV 50 cm)
- ④ Summary

# Jagiellonian Positron Emission Tomograph

2012

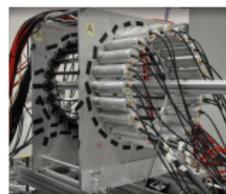


Characterize scintillator properties

*Energy resolution, fit time, ...*

192 strips

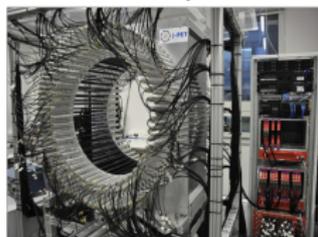
2014



24 strips

Data acquisition for **multi-modules**

2016



Current version

**Tests on discrete symmetries**

2018

Modular PET – **ready for first data campaign**

- **2012** : First prototype with 2 plastic strips read by vacuum photomultipliers.
- **2014** : Data acquisition was successfully tested with multiple module system.
- **2016** : Prototype optimized to study the decays of positronium atoms
- **2018-2021** : Modular prototype - major changes in terms of SiPMs readout.

# Key features

- **192 detection modules** arranged in 3 Layers.
- Each module is made made of **plastic scintillators** ( $50 \times 1.9 \times .7 \text{ cm}^3$ ) and **2 photomultipliers** on each end.
- Trigger less and reconfiguration DAQ
- **Time Over Threshold (TOT)**  
*Measure of energy deposition\**
- Multiple photon detection in a single event
- Ang. reso. ( $\approx 1^\circ$ )  
Good time reso. ( $\approx 200 \text{ ps}$ )

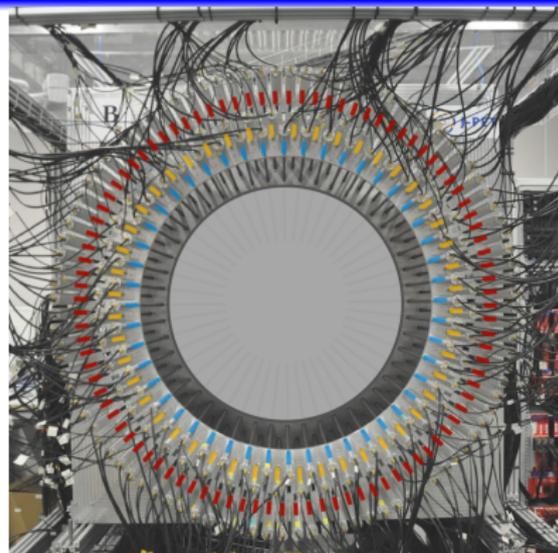
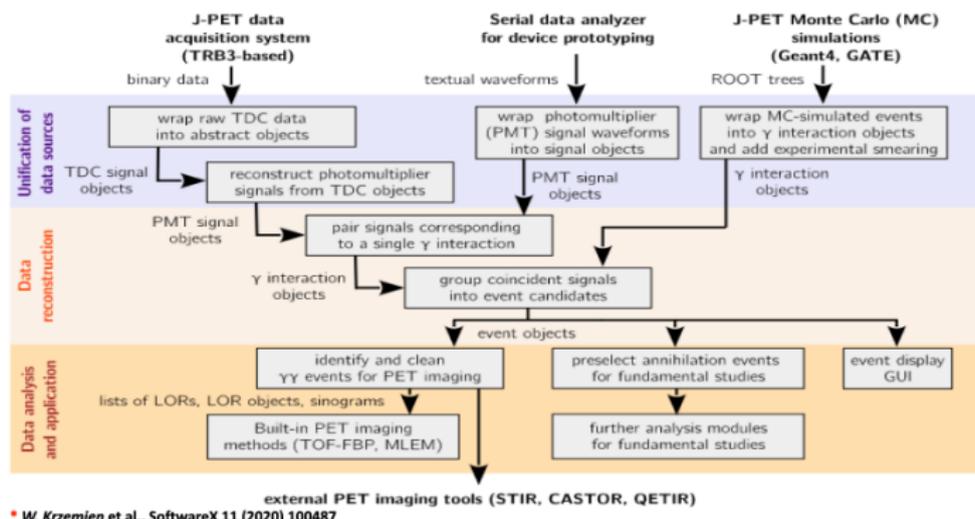


Figure: 3 Layers prototype

$$\text{Eres.}(\sigma_E/E) = 0.044/\sqrt{E(\text{MeV})}$$

\* S. Sharma., P. Moskal et al., EJNMMI Physics 7, 39 (2020)

# Data Acquisition and Analysis : J-PET framework\*

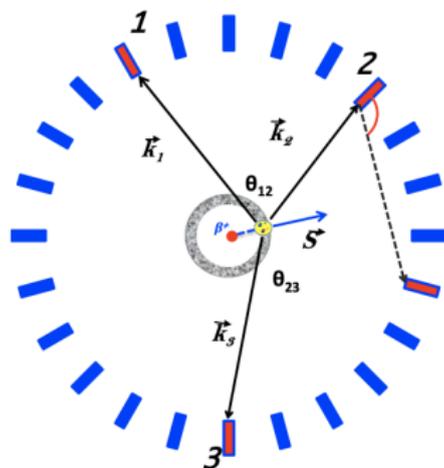


- J-PET Analysis Framework can be categorized in three sequential steps : DAQ (FPGA based), reconstruction of signal events and data analysis
- Mainly written in **C++11** using heavily the **ROOT** and **BOOST** libraries
- Dedicated MC simulations based on **Geant4** toolkit and **GATE** package

# Positronium Decays : Applications in **Fundamental** and **Medical** physics

- First time detected in Gas by Martin Deutsch  
**Nobel prize in 1956 for discovering Ps**
- Hydrogen like atom without nuclei : purely leptonic object  
**particle :  $e^-$  and anti-particle :  $e^+$**
- Eigenstate of C,P,CP operators
- Undergoes self-annihilation into gamma quanta.  
**Number of annihilated photons followed the charge parity conservation.**
- Formed in two gnd. states:  
para-Positronium(p-Ps - .125 ns)      ortho-Positronium(o-Ps - 142 ns)  
( $S=0, m_z=0$ ).      ( $S=1, m_z=-1, 0, 1$ )  
Even no of photons 2,4,.. **Charge Conj.**      Odd no of photons 3,5,..
- J-PET qualifies to perform the tests on discrete symmetries
- **Positronium imaging** in human body (novel concept with J-PET)

# Tests on discrete symmetries in the decays of o-Ps atoms



## Positronium production chambers



## Target chambers

## Table: Operators

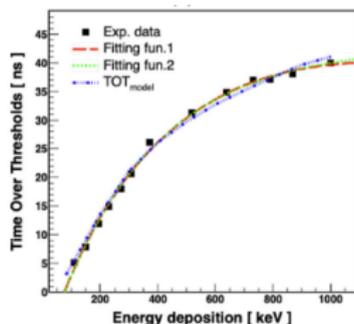
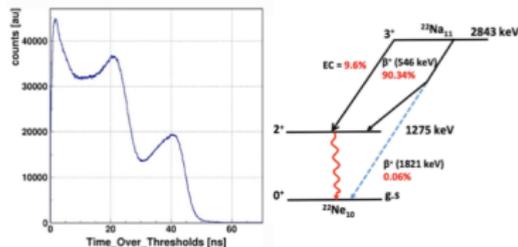
Odd symmetric	C	P	T	CP	CPT
$\vec{S} \cdot \vec{k}_1$	+	-	+	-	-
$\vec{S} \cdot (\vec{k}_1 \times \vec{k}_2)$	+	+	-	+	-
$(\vec{S} \cdot \vec{k}_1)(\vec{S} \cdot (\vec{k}_1 \times \vec{k}_2))$	+	-	-	-	+

- Odd symmetry operators can be constructed using momentum vectors of annihilation photons ( $\vec{k}_i$ ) and Spin of Ps

# Control Spectra for data analysis

## Time Over Thresholds

measure of energy depositions

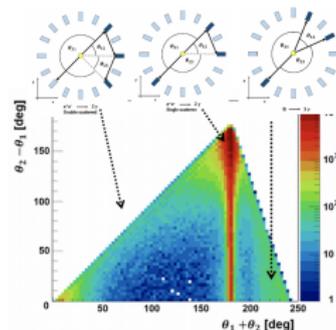


EJNMMI Physics 7, 39 (2020);  
K. Dulski et al. NIM A(in press)  
S. Sharma (UJ)

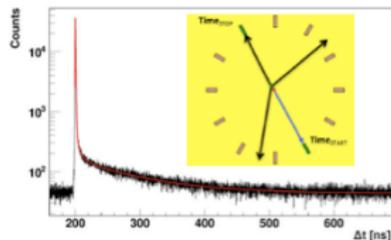
TIPP2021

## Azimuth angles

Angular correlation b/w anni. photons



## Life time of Ps atoms

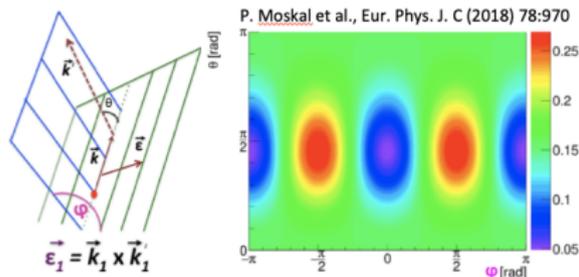


Acta Phys. Pol. B 48:10(2017)  
Hyperfine Inter. 2018(239:40)

25.05.2021

# Tests on discrete symmetries using the photons' polarization

- ◇ J-PET allows to register primary and scattered photon
- ◇ Photon (low energetic) most likely scattered in plane  $\perp_{e_r}$  to electric vector (dir<sup>n</sup> of the linear polarization).
- ◇ Photon's polarization direction -



With access to *photon polarization direction*, more operators are proposed\*:

Table: Operators

Odd symmetric	C	P	T	CP	CPT
$\vec{S} \cdot \vec{k}_1$	+	-	+	-	-
$\vec{S} \cdot (\vec{k}_1 \times \vec{k}_2)$	+	+	-	+	-
$(\vec{S} \cdot \vec{k}_1)(\vec{S} \cdot (\vec{k}_1 \times \vec{k}_2))$	+	-	-	-	+
<b>New Operators unique with J-PET = <math>\vec{\epsilon}</math></b>					
$\vec{k}_1 \cdot \vec{\epsilon}_2$	+	-	-	-	+
$\vec{S} \cdot \vec{\epsilon}_1$	+	+	-	+	-
$\vec{S} \cdot (\vec{k}_2 \times \vec{\epsilon}_1)$	+	-	+	-	-

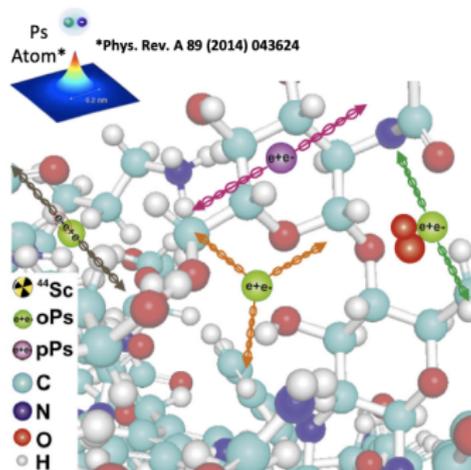
\*Acta Phys. Pol. B 47, 509(2016)

# Positronium imaging in medical physics

- During PET imaging in **30-40%** cases,  $e^+e^-$  annihilation occurs in the tissues via forming the Ps atoms.
- Out of total annihilation, 0.5 % contribution comes from the  $e^+e^- \rightarrow 3\gamma$  (via formation of meta-stable o-Ps atoms).
- Recent studies(PALS based) has shown that Avg. lifetime of o-Ps atoms (142 ns in vacuum) can be different depending on the **healthiness of tissues** (e.g. for normal tissues, avg. lifetime is generally more than the cancerous tissues) and thus can reveal very **important information about the stage/metabolic disorders** of human tissue.
- Considering relatively low probability of such events, it seems **feasible only** in the context of total-body PET

imaging(higher sensitivity and with good time resolution).

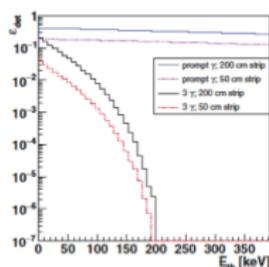
- Requires **radiopharmaceuticals** emitting a **prompt photon** (eg  $^{44}\text{Sc}$ )



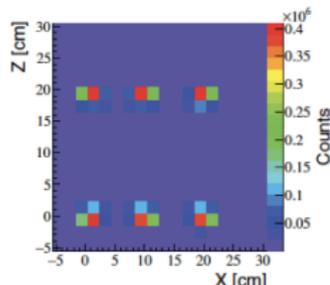
P. Moskal and E.L. Stepien, PET Clinics 15:4 (2020)439-452

# Feasibility study of Ps imaging with J-PET\*

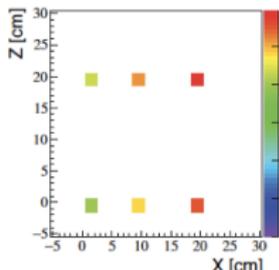
- MC simulations were performed for the **imaging** of **o-Ps mean lifetime** using ideal geometry of J-PET tomograph constructed of plastic scintillators ( $7 \times 19 \times 500 \text{ mm}^3$ ).
- Registration efficiency (AFOV 50cm, 200 cm) as a function of energy dep. threshold was simulated (a) for 511 keV and prompt photon (1.16 MeV for  $^{44}\text{Sc}$ )
- Annihilation points** (b) were reconstructed based on the **trilateration** method\*\*
- Six point like sources with lifetime varying in between 2 - 3 ns (voxel size  $2 \times 2 \times 2 \text{ cm}^3$ ) were simulated (c) as described in work\*.



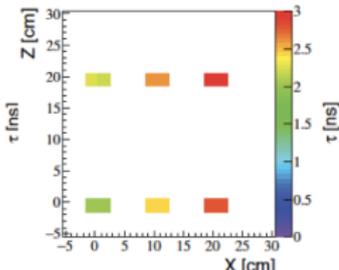
(a) Registration efficiency



(b) Rec. ann. points in spat. Coordinates



(c) Gen. o-Ps life distributions



(d) Rec. o-Ps life distributions

P. Moskal et al., Phys. Med. Biol. 64 (2019) 055017

\*D. Kaminska et al., Euro. Phys. J. C 76 (2016) 445

\*\*A. Gajos et al., Nucl. Instrum. Meth. A 819 (2016) 54–9

# Modular J-PET : *Portable tomograph (AFOV 50cm)*

## Figure: Digital J-PET

- Composed of **24 individual modules**
- Each module is made of **13** plastic scintillators ( $50 \times 24 \times 6 \text{ cm}^3$ )
- Each side of scintillator is read out by **matrix of SiPMs**
- Modular construction allows to configure as **one layer** (24) or **multiple layers** (e.g., 8, 16 and thus requirement specific)
- Modules can be operated individually enabling to utilize as multi-role detector
- Easy to transport (full barrel around 60 kg)

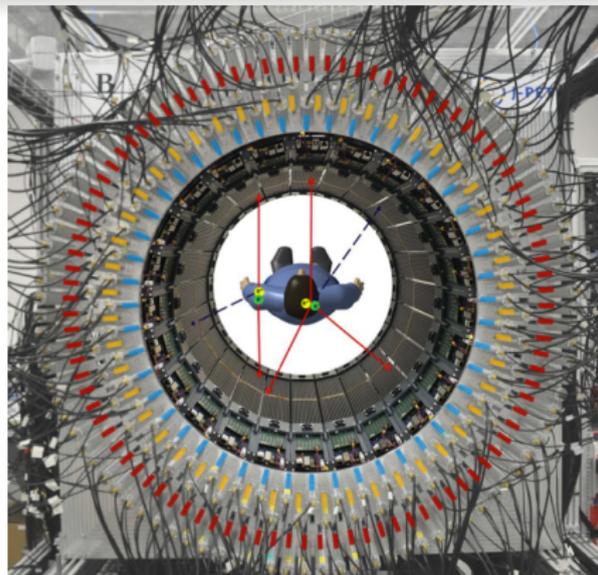


Figure: Modular+3layers

- ✳ J-PET is a **cost-effective alternative** to the crystal based PET tomograph.
- ✳ **Modular construction** of detection units allows the flexible

use in medical and particle physics.

- ✳ Modular prototype with AFOV 50 cm is already commissioned and started to collect the data as a standalone layer.
- ✳ 24 modules can be reconfigured in multiple layers and can be transported to use in other experimental facilities which demands the the detection of  $e^+e^-$  anni. in full phase space.
- ✳ It is foreseen that using the modular J-PET with 3 layers prototype will enhance the efficiency by an order of magnitude.



# J-PET Collaboration

# THANK YOU

More details : <http://koza.if.uj.edu.pl/>