## $3\gamma$ tomography with J-PET

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# $e^+e^-$ annihilation with additional photon from $\beta^+$ emitter deexcitation

- 2 annihilation photons are created back-to-back
- deexcitation photon momentum is independent
- the additional photon is used to increase imaging resolution

08.06.2017 2 / 15 γ1 γ2 γ2 γ2 γ2 γ3 γ2 γ2 γ3 γ2 γ3

 $\begin{array}{l} \mbox{Ortho-positronium tomography with} \\ \mbox{oPs} \rightarrow 3\gamma \mbox{ annihilation} \end{array}$ 

- momenta of three photons created in o-Ps decay are co-planar
- ortho-positronium (o-Ps) lifetime in tissue strongly depends on inter-cellular spaces' size
- morphological imaging possible through determination of o-Ps lifetime<sup>1</sup>

Material	No Ps formed <sup>2</sup>	Water <sup>2</sup>	IC3100 <sup>3</sup>	XAD-4 <sup>3</sup>
$f_{3\gamma} = \sigma_{3\gamma} / \sigma_{2\gamma}$	0.27%	0.52%	16.9%	28.9 %

<sup>1</sup>A. Gajos, E. Czerwiński, D. Kamińska, P. Moskal, patent PCT/PL2015/050038

<sup>2</sup>K. Merkurio et al., Phys. Med. Biol. **51**, N323 (2006)

<sup>3</sup> B. Jasińska et al., Acta Phys. Polon. B **47**, 453 (2016)

### J-PET detector





For a details see a talk by Sz. Niedźwiecki at Applied physics: Medical Applications, Monday



J-PET	Standard PET	
Polymers	Crystals	
Low granularity	High granularity	
Low efficiency	High efficiency	
High acceptance	Low acceptance	
Compton scattering	Photoeffect	
Time domain	Energy domain	
Digital electronics	Analog electronics	







# $3\gamma\text{-}\mathsf{PET}$ technique with the J-PET detector





- Large acceptance offered by the J-PET apparatus allows for simultaneous recording of both annihilation photons as well as the deexcitation photon
- PET imaging resolution strongly depends on TOF resolution along the line of response (LOR)
- Information on the deexcitation photon can be used to improve resolution along LOR





- Ortho-positronium (o-Ps) lifetime in tissue strongly depends on inter-cellular spaces' size
- The detection of 3γ annihilation photons carries information about the environment with which the positron interacts
- Morphological imaging possible through determination of o-Ps lifetime



www.web-books.com/eLibrary/Medicine/Appendix/PETscan.jpg



Comparison between o-Ps lifetime ( $\tau$ ) and a diameter of free volume (D). Solid line and red points shows theoretical prediction and experimental data, respectively. Figure is adapted from *R. Zaleski*, Nukleonika **60** 795 (2015)

### Simulations

- i) positron emission and thermalisation in the target material.
- ii) angular and energy distributions of gamma quanta originating from ortho-positronium annihilation.
- iii) Compton interactions of emitted gamma quanta in the detector built from plastic scintillators,
- iv) determination of gamma quanta hit-position and hit-time in the detector with experimentally determined resolutions.
- multiple scattering and v) accidental coincidences.
- vi) reconstruction of registered gamma quanta fourmomenta





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-PET



 $\Uparrow$  Geometry already build and tested



- 4-th (deexcitaion) photon momentum is not correlated with the other three
- o-Ps  $\rightarrow 3\gamma$  decay and deexcitation photon emission differ by distance and time related to free  $e^+$  path and positronium life



#### ↑ Simulated geometry







A. Gajos et al. (J-PET) NIM A819, 54 (2016)

1 Find the decay plane containing the 3 hits in the J-PET barrel

- 2 Transform the hit coordinates to a 2D coordinate system in the decay plane  $(X_i, Y_i, Z_i, T_i) \rightarrow (X'_i, Y'_i, 0, T'_i)$
- 3 For each of the recorded  $\gamma$  hits define a circle of possible origin points of the incident photon assuming o-Ps decay at time t
- 4 Find the decay point (x', y') in the decay plane and time t as an intersection of 3 circles by solving the following equation system:

$$(T_i - t)^2 c^2 = (X'_i - x')^2 + (Y'_i - y')^2, \quad i = 1, 2, 3$$

where: x', y', t - unknowns,  $T_i$  - time of i-th hit,  $X'_i, Y'_i$  - coordinates of the i-th hit in the barrel expressed in the decay plane coordinates

**5** Transform (x', y', t) of the decay point back to the detector 3D coordinate system

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### Spatial and time resolution of o-Ps decay point

The resolution of o-Ps decay obtained with the presented reconstruction method depends predominantly on the timing resolution of  $\gamma$  hits in scintillator strips.



A. Gajos et al. (J-PET) NIM A819, 54 (2016)

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## Ortho-positronium lifetime resolution

The ortho-positronium lifetime can be estimated as:





 $\sigma(T_{hit})$  [ps]

- $t_0$  reconstructed o-Ps decay time
- $L_{\gamma}^{deexc.}$  is calculated using reconstructed o-Ps decay point



# Morphological imaging





- $\bullet\,$  cylindrically shaped  $\beta^+$  emitter is localized in the center of the detector
- radioactive source is uniformly distributed along the cylinder
- ortho-positronium lifetime changes with the azimuthal angle
- values of oPs lifetime in plasma or hematocrits is within range 1.7-2.4 ns



Z [cm]



Morphological imaging

# () J-PET



#### Summary



- The J-PET detector can be used for multi-photon positron emission tomography imaging
- The standard TOF-PET spatial resolution can be improved by using information from de-excitation photon
- A novel imaging technique based on ortho-positronium annihilation into three-photons is based on the fact that the properties of ortho-positronium atom depend strongly on the size of the free volumes between molecules
- The latter technique may be used as an indicator of the stage of development of metabolic disorders

# Thank you for your attention