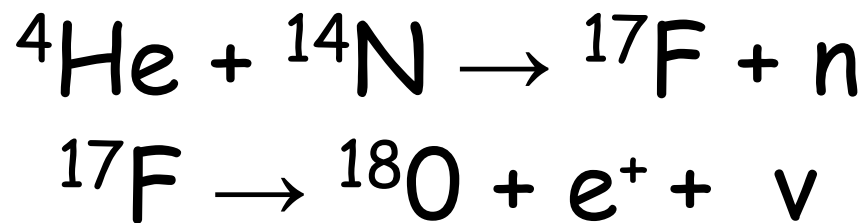


Radiological
Laboratory
in Warsaw
(1934)



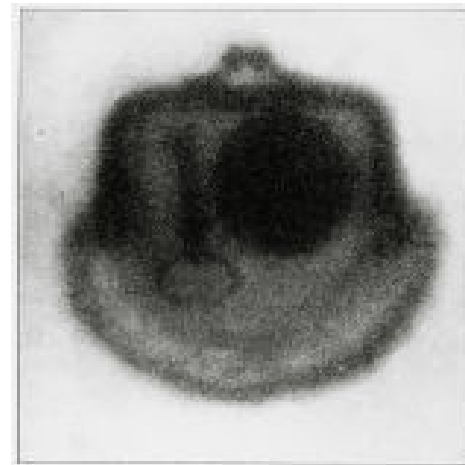
Marian Danysz



Formal leader of the Radiological
Laboratory in Warsaw



A girl from Warsaw

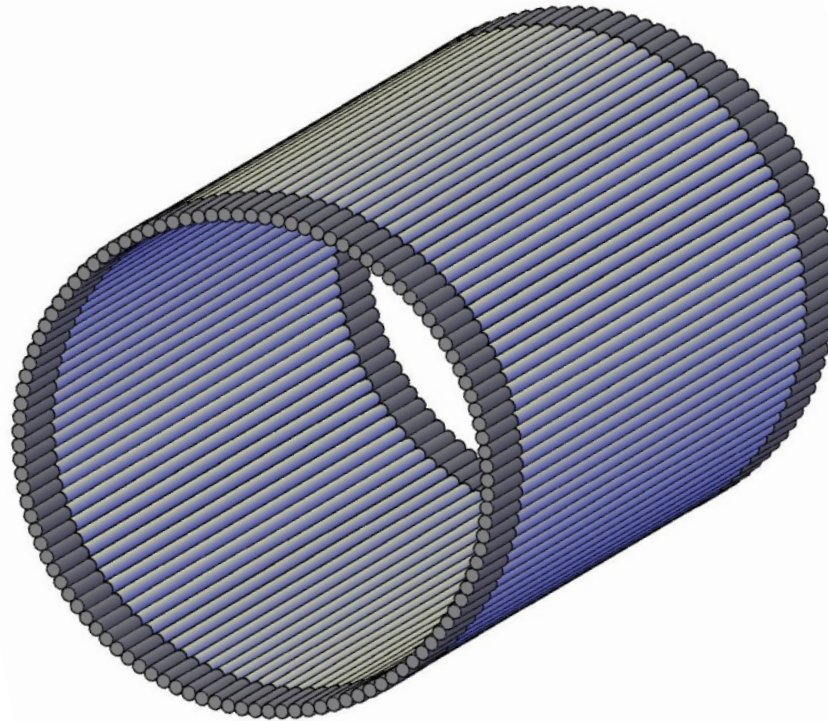


„Radiograph”
taken by
Maria Curie
by exposing
a purse to radium.

[http://www.galloim
ages.co.za/](http://www.galloim
ages.co.za/)



Jagiellonian PET project



II Symposium on Positron Emission Tomography
Cracow, 21-24 September 2014

Pawel Moskal

Jagiellonian University, Cracow, Poland

for and on behalf of the J-PET collaboration

Supported by Polish National Center for Development and Research
and Foundation for Polish Science



IMAGE

Experimental Group of Advanced Medical Imaging
PET and polarized-MRI

- **Jagiellonian PET (J-PET)**

Jagiellonian University, National Center of Nuclear Reserach



IMAGE

Experimental Group of Advanced Medical Imaging
PET and polarized-MRI

- **Jagiellonian PET (J-PET)**

Jagiellonian University, National Center of Nuclear Reserach

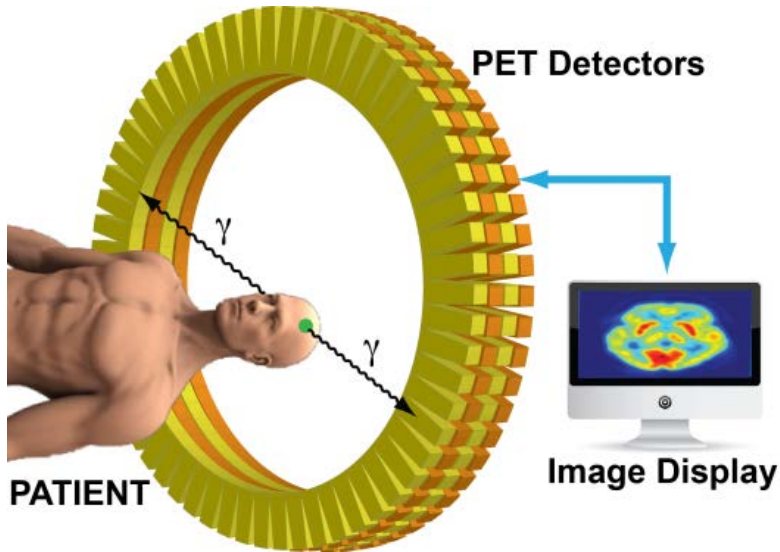




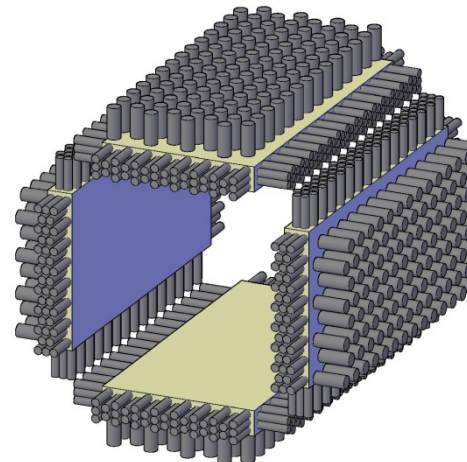
Novel detector systems for the Positron Emission Tomography aiming at the simultaneous, whole body imaging

<http://koza.if.uj.edu.pl>

General scheme of the currently used PET tomographs

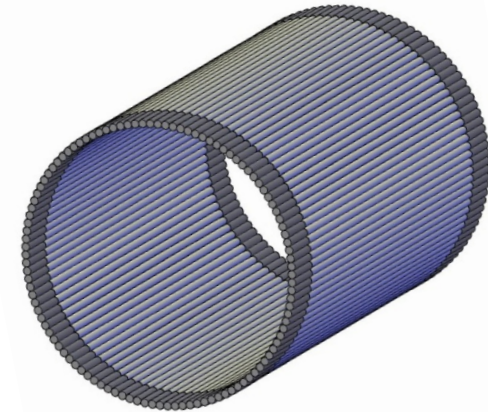


MATRIX-PET



PCT/PL2010/000061

STRIP-PET



PCT/PL2010/000062

Utterly new paradigm

Crystal



Polymer

Energy



Timing

High granularity



Low granularity

High efficiency



Low efficiency

Photoeffect



Compton scattering

Low acceptance



High acceptance

Analog electronics



digital sampling

triggering



triggerless DAQ

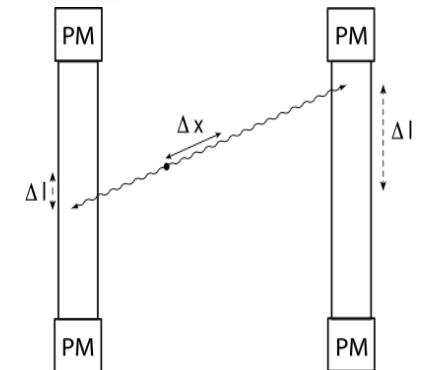
Currently all PET are based on crystals

PHILIPS → LYSO

SIMENS → LSO

GE Healthcare → BGO

$$\Delta l = \frac{(t_2 - t_1) \cdot v}{2} \cong \frac{(t_2 - t_1) \cdot c}{4}$$



$$\Delta x = \frac{(t_l - t_r) \cdot c}{2} \implies \Delta x = \frac{\Delta t}{2} \cdot c$$



Type: LSO / LYSO / BGO / polymer scintillator

Price per cm³: 86 / 86 / 35 / 1

Polymer scintillators can be easily produced in large sizes and various shapes

PHILIPS → LYSO

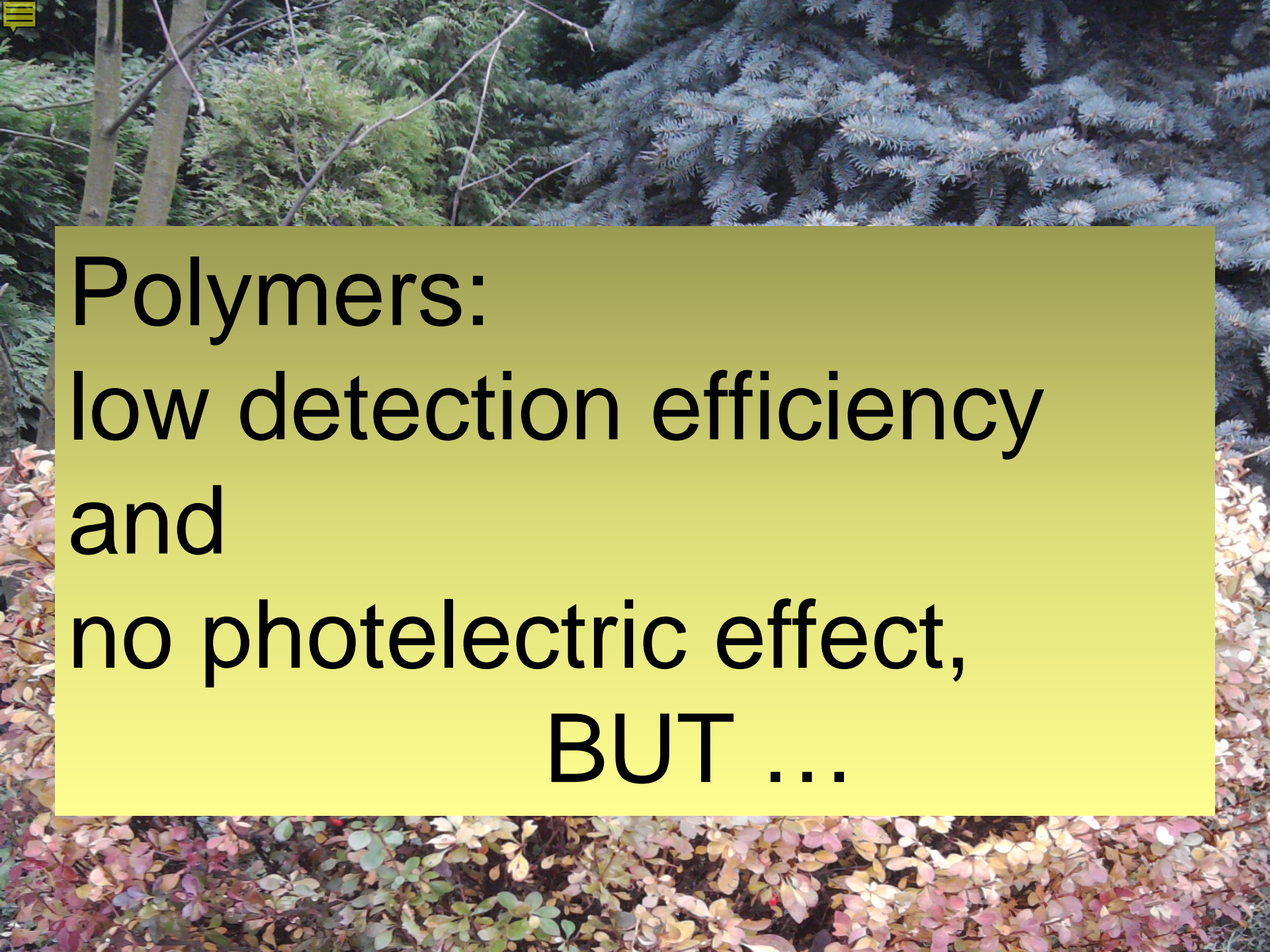
SIMENS → LSO

GE Healthcare → BGO

Why polymers were not considered
so far as a material for PET detectors ?

for the 2.5 cm layer the efficiency for the registration of events selected to reconstruct the image is for the plastic scintillator by a factor of about 20 smaller in relation to the BGO crystals and about 40 times less compared to the LSO crystals

name	type	density [g/cm³]	decay time [ns]	photons/ MeV	mean free path [cm]
BGO	crystal	7.13	300	6000	1.04
GSO	crystal	6.71	50	10000	1.49
LSO	crystal	7.40	40	29000	1.15
NE102A	polymer	1.032	2.4	10000	10.2
BC404	polymer	1.032	1.8	10000	10.2
RP422	polymer	1.032	1.6	10000	10.2

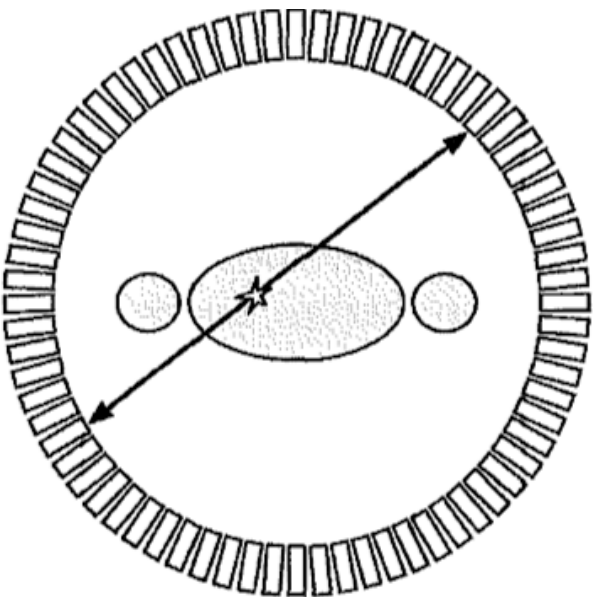
The background of the slide is a photograph of a forest. In the upper right, there are dense evergreen trees with blue-green needles. In the lower half, there are deciduous trees with autumn-colored leaves in shades of red, orange, and yellow. A yellow rectangular box is overlaid on the center of the image, containing black text.

Polymers:
low detection efficiency
and
no photoelectric effect,
BUT ...

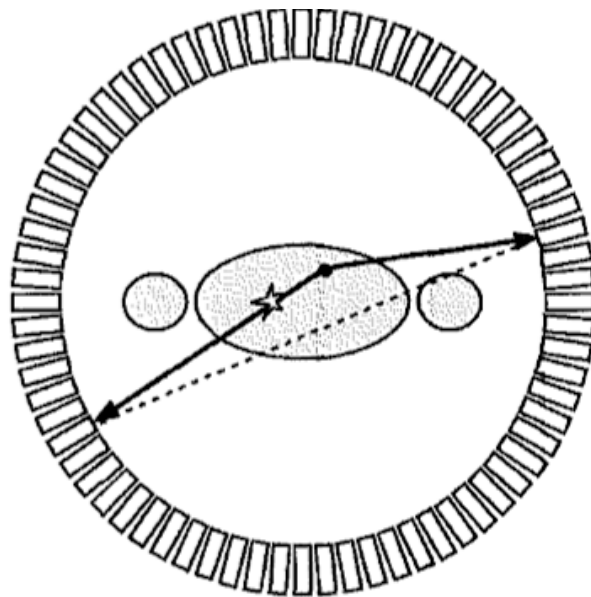


EVENTS

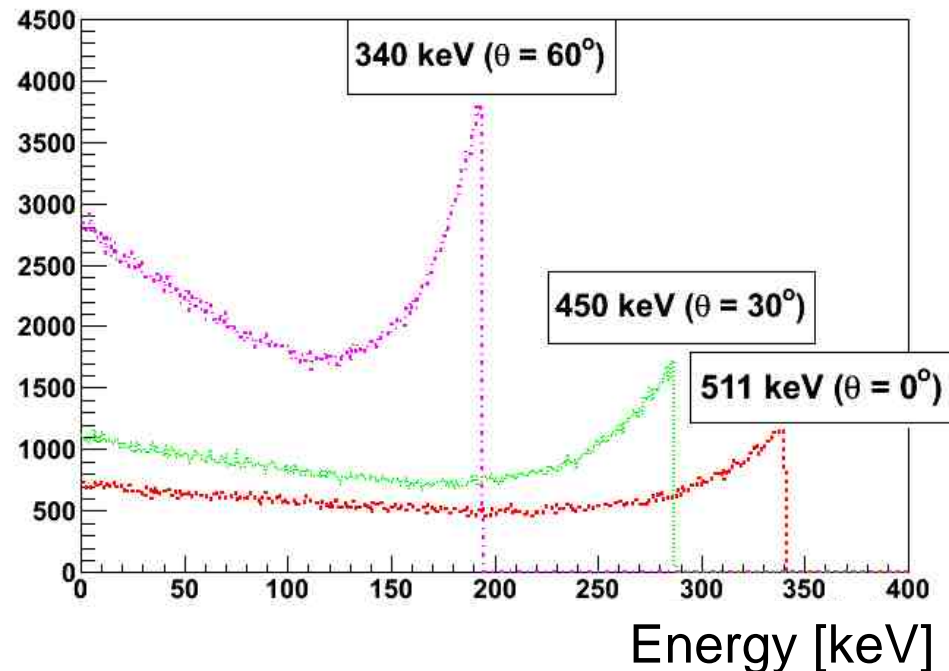
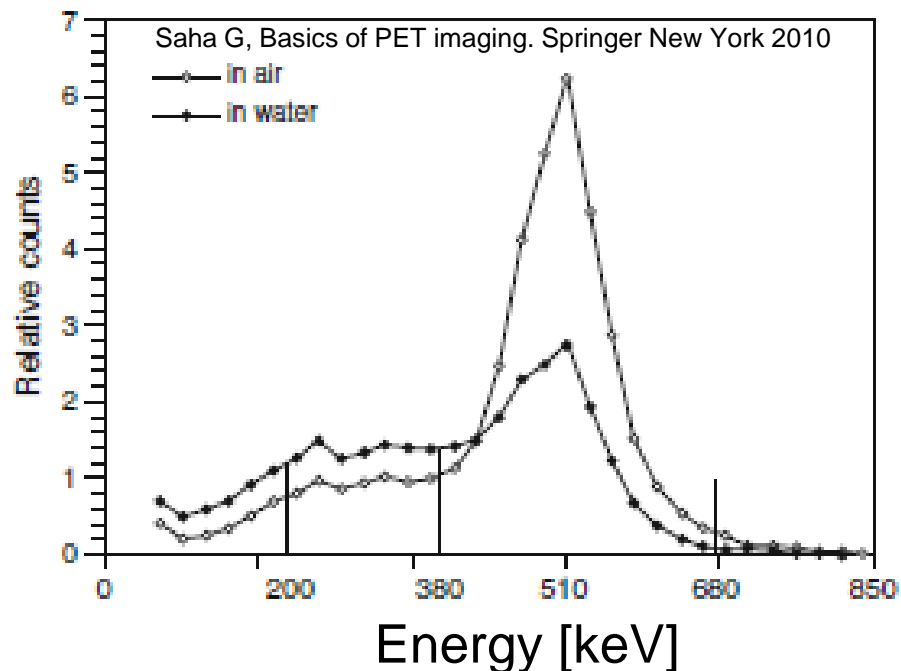
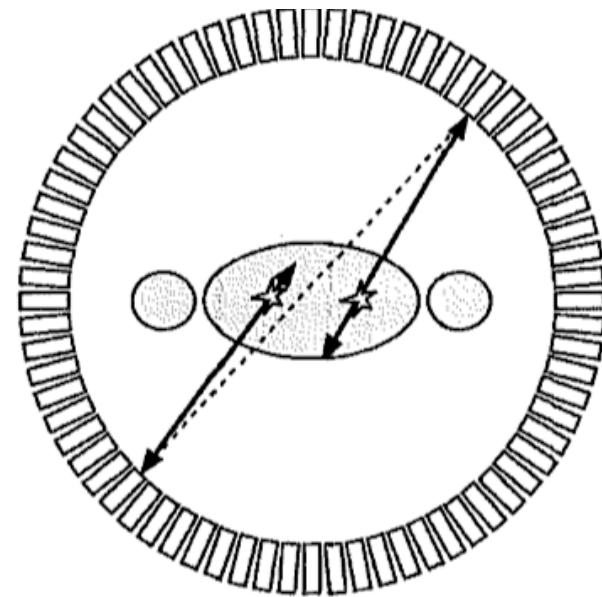
„true”



„scattered”



accidental

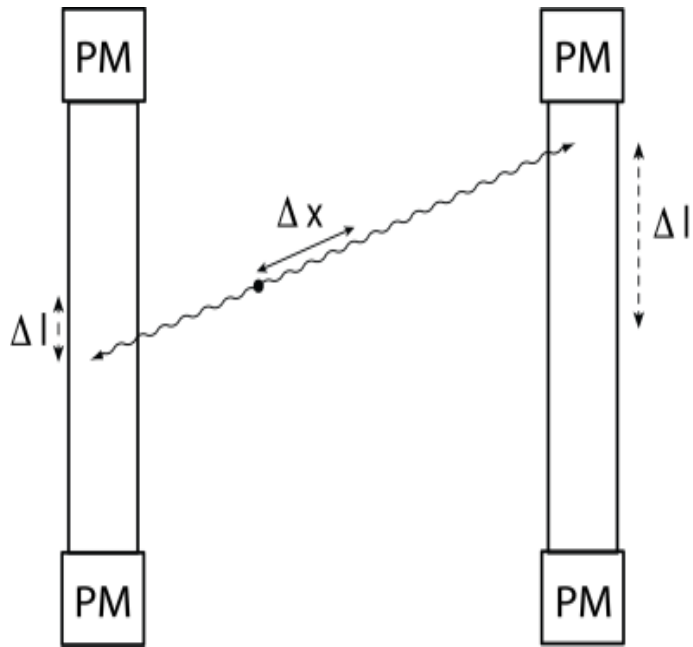


LIGHT SIGNALS FROM POLYMERS ARE MUCH „FASTER” !!!

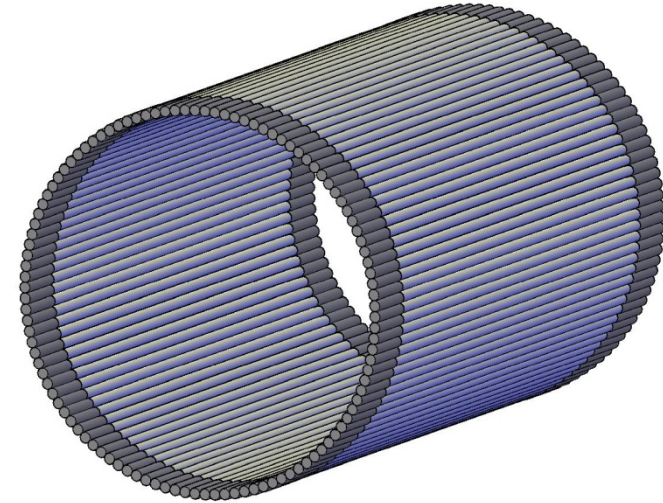
name	type	density [g/cm³]	decay time [ns]	photons/ MeV	mean free path [cm]
BGO	crystal	7.13	300	6000	1.04
GSO	crystal	6.71	50	10000	1.49
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NE102A	polymer	1.032	2.4	10000	10.2
BC404	polymer	1.032	1.8	10000	10.2
RP422	polymer	1.032	1.6	10000	10.2

J-PET (Jagiellonian PET)

$$\Delta l = (t_2 - t_1) v / 2$$



$$\Delta x = (t_l - t_r) c / 2$$



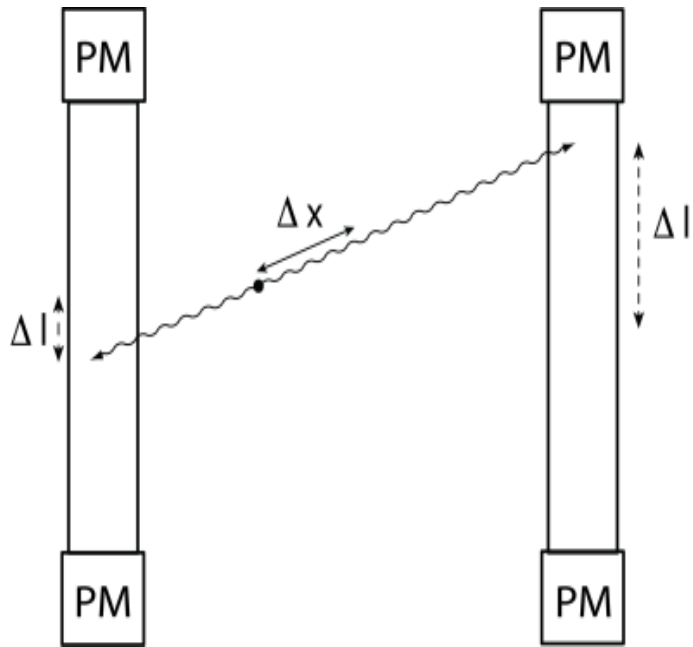
Lets take advantage of TIME resolution not only for TOF but also for the determination of hit positions

Thus for example:

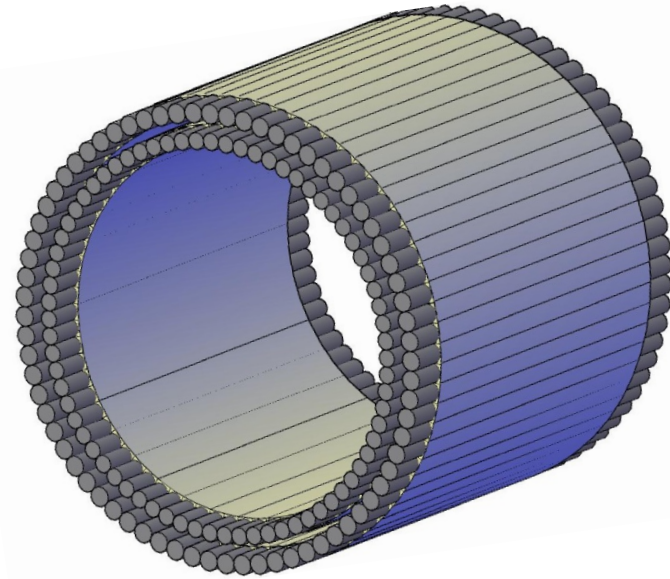
$$\text{FWHM}(\Delta t) = 100\text{ps} \rightarrow \text{FWHM}(\Delta l) = 0.7\text{cm} \rightarrow \text{FWHM}(\Delta x) = 1\text{cm}$$

J-PET (Jagiellonian PET)

$$\Delta l = (t_2 - t_1) v / 2$$



$$\Delta x = (t_l - t_r) c / 2$$

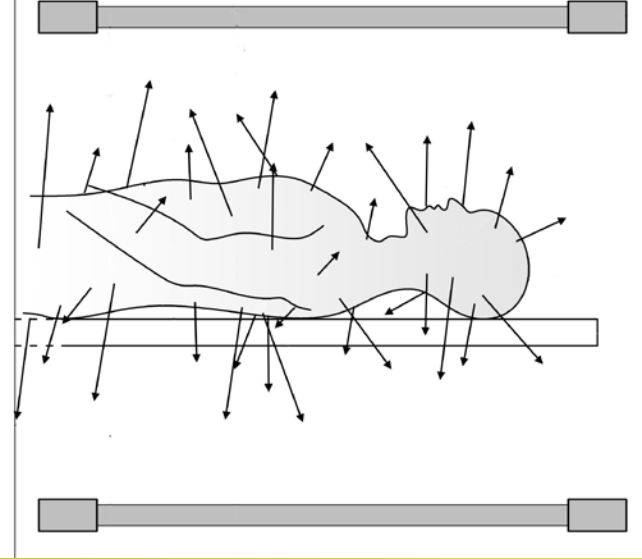
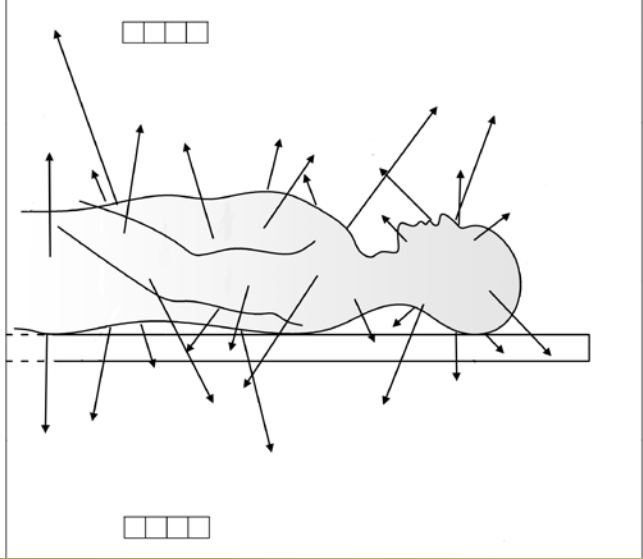


$$\text{FWHM}(\Delta l) \approx \text{FWHM}(\Delta t) * c/4$$

$$\text{FWHM}(\Delta x) \approx \text{FWHM}(\Delta t) * c / 2\sqrt{2}$$

Thus for example:

$$\text{FWHM}(\Delta t) = 100\text{ps} \rightarrow \text{FWHM}(\Delta l) = 0.7\text{cm} \rightarrow \text{FWHM}(\Delta x) = 1\text{cm}$$



It is important to note that the cost of J-PET does not increase with the increases of the FOV

$\epsilon^2 = 20$ to 40 smaller efficiency

But

2D \rightarrow 3D ----- $>$ factor of ~ 5

600ps \rightarrow 100ps – 200ps \rightarrow factor of 6 -- 3

1m instead of 20cm ----- $>$ factor of 9

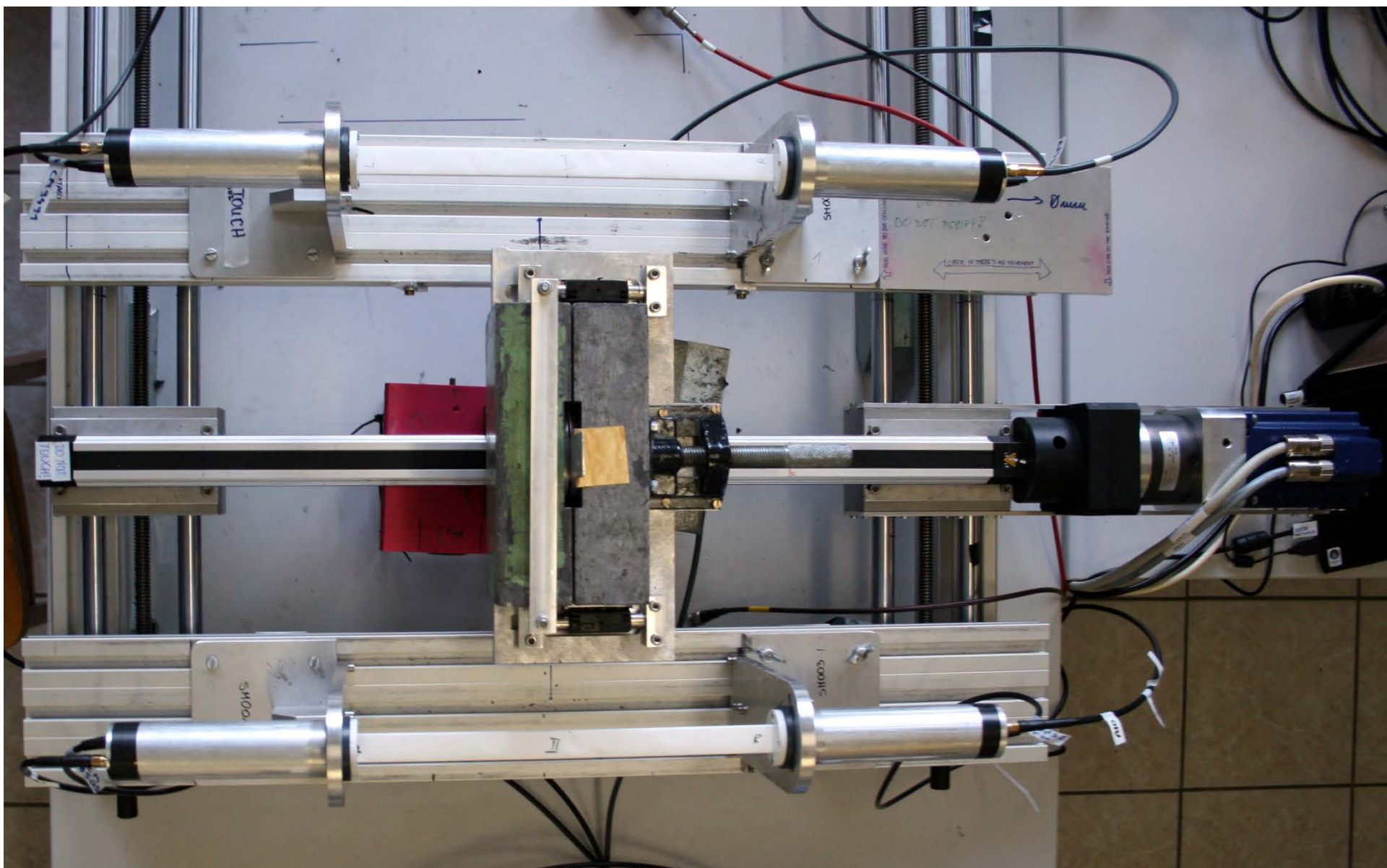
N layers in the strip-PET \rightarrow factor **N^2**

For $N=1$ --- \rightarrow total factor of ~ 200

Lower dose by factor of 7

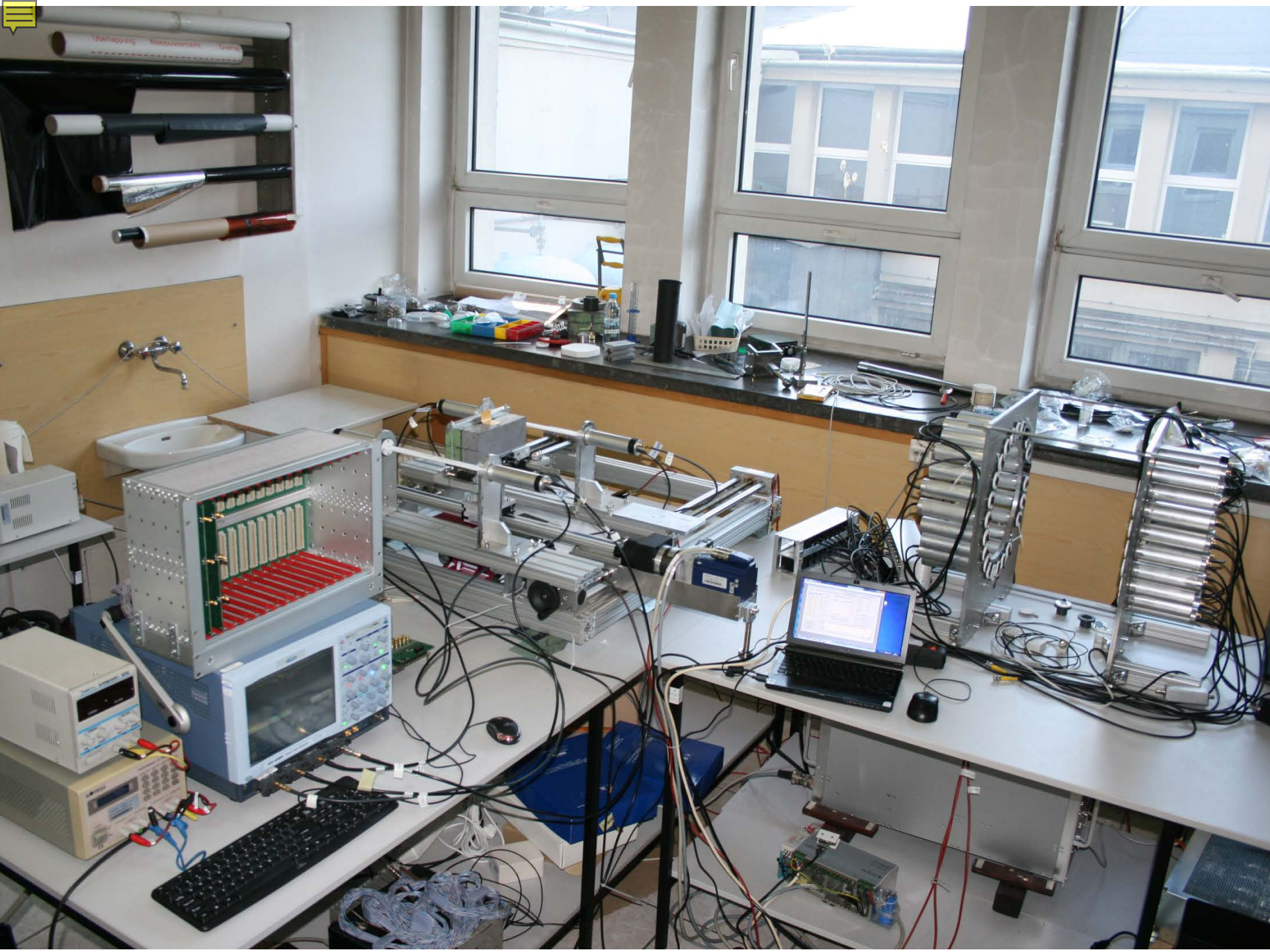
Accidental coincidences less by factor of about 1000

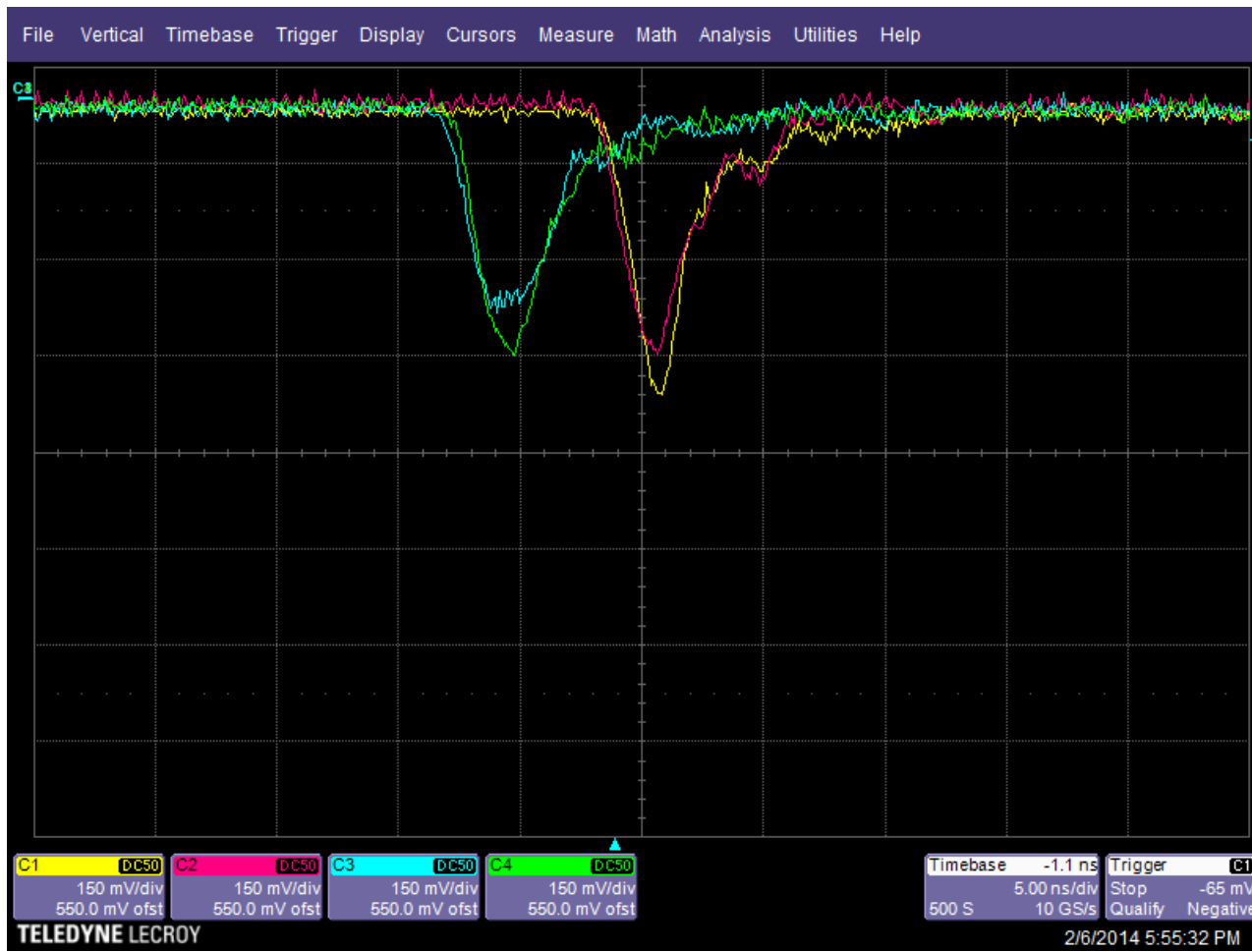
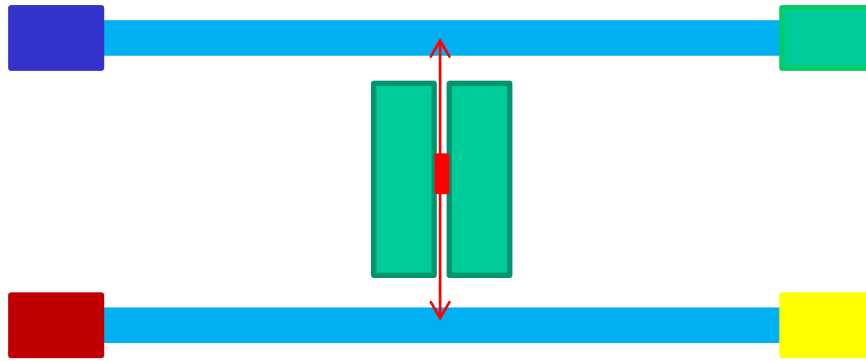
$(\epsilon * 7)^2$

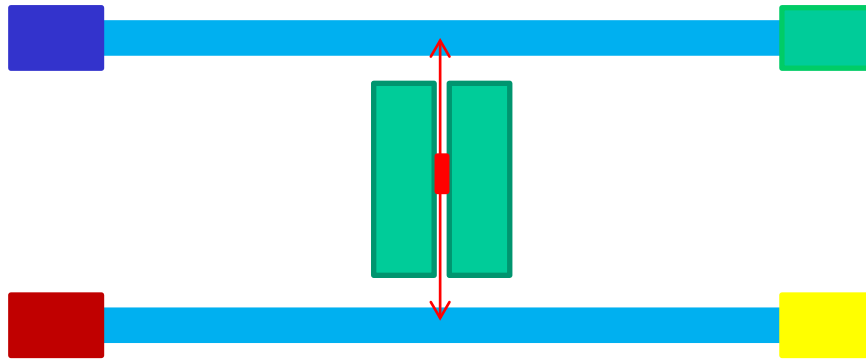


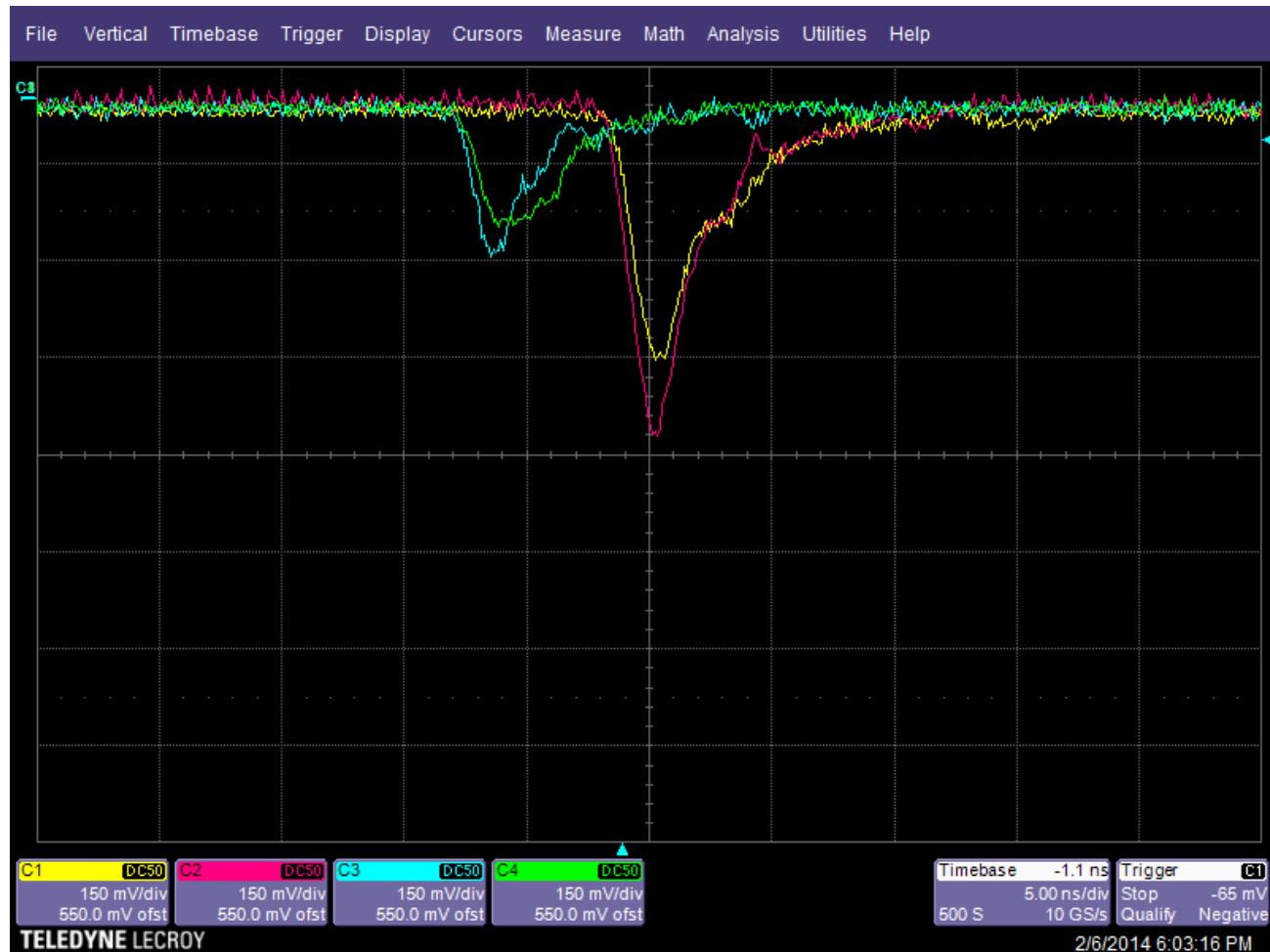
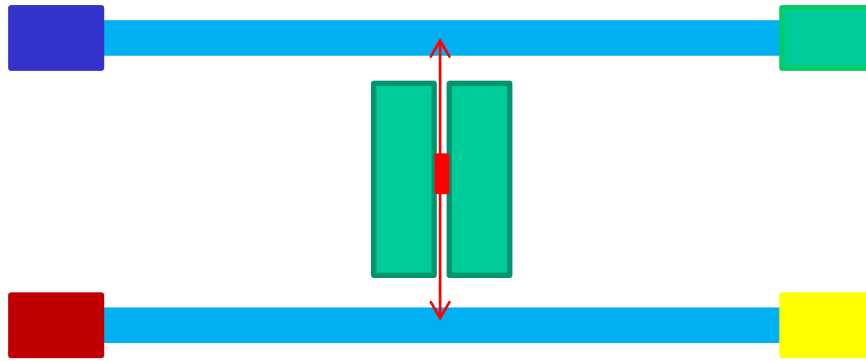
J-PET: Nucl. Instr. & Meth. A764 (2014) 317

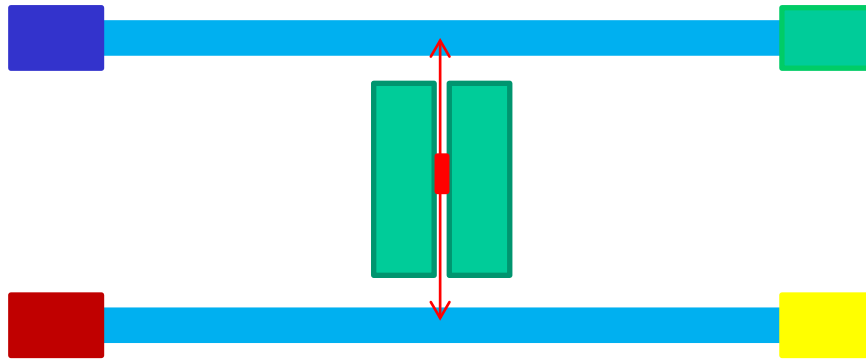
J-PET: Nucl. Instr. & Meth. A764 (2014) 186

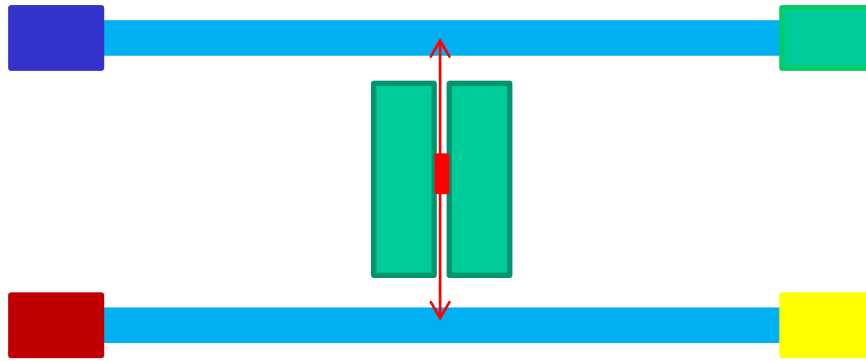


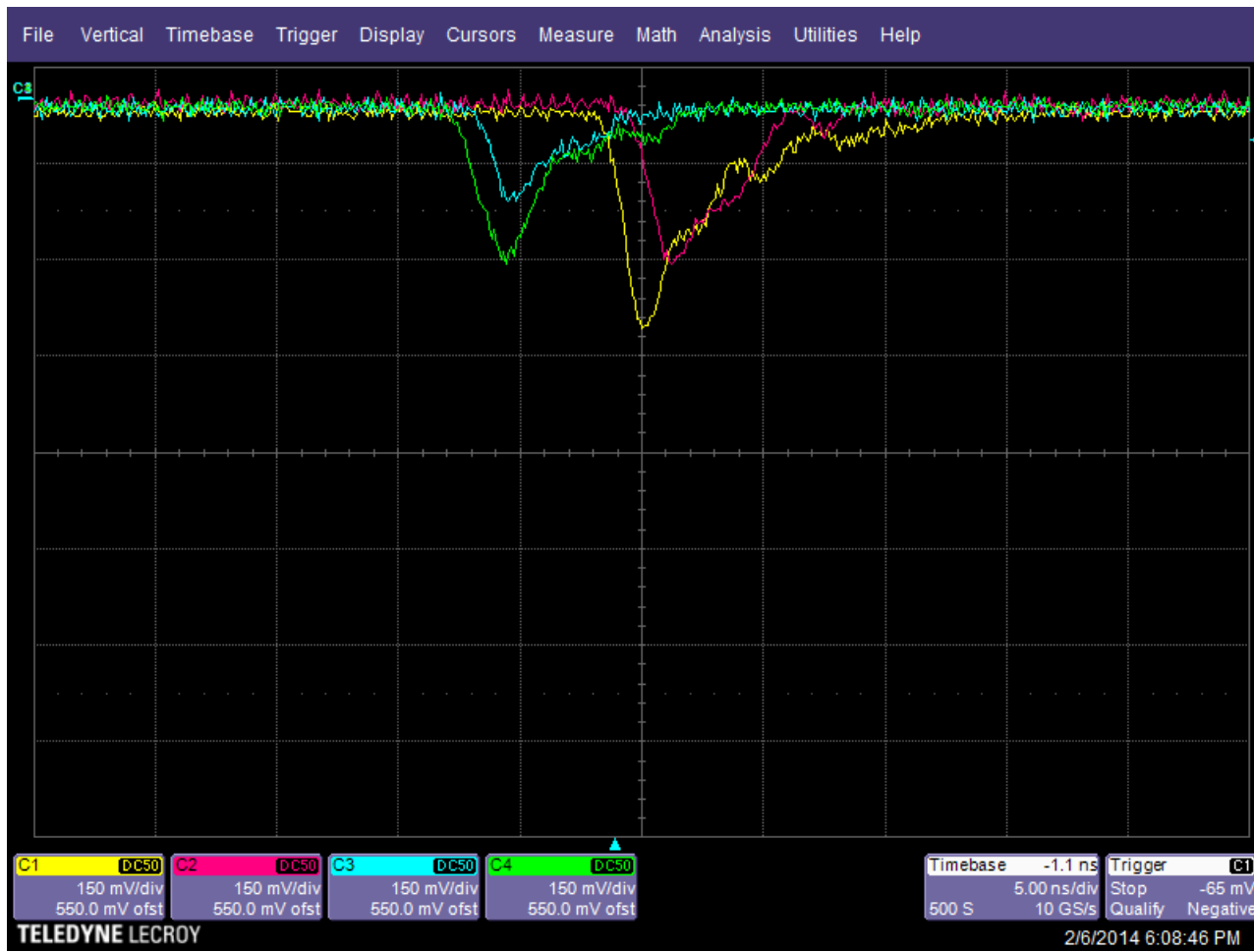
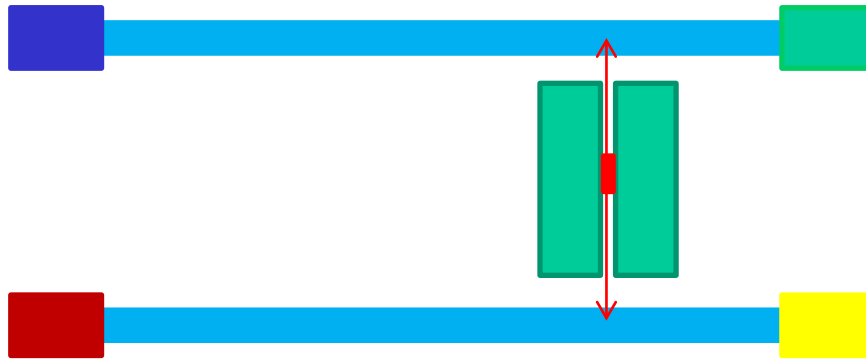


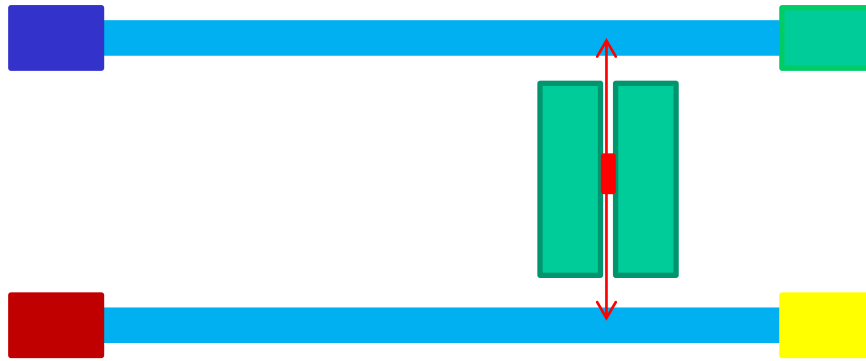


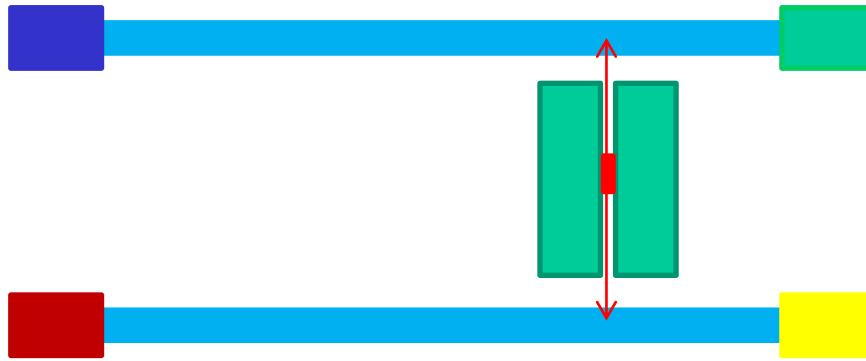


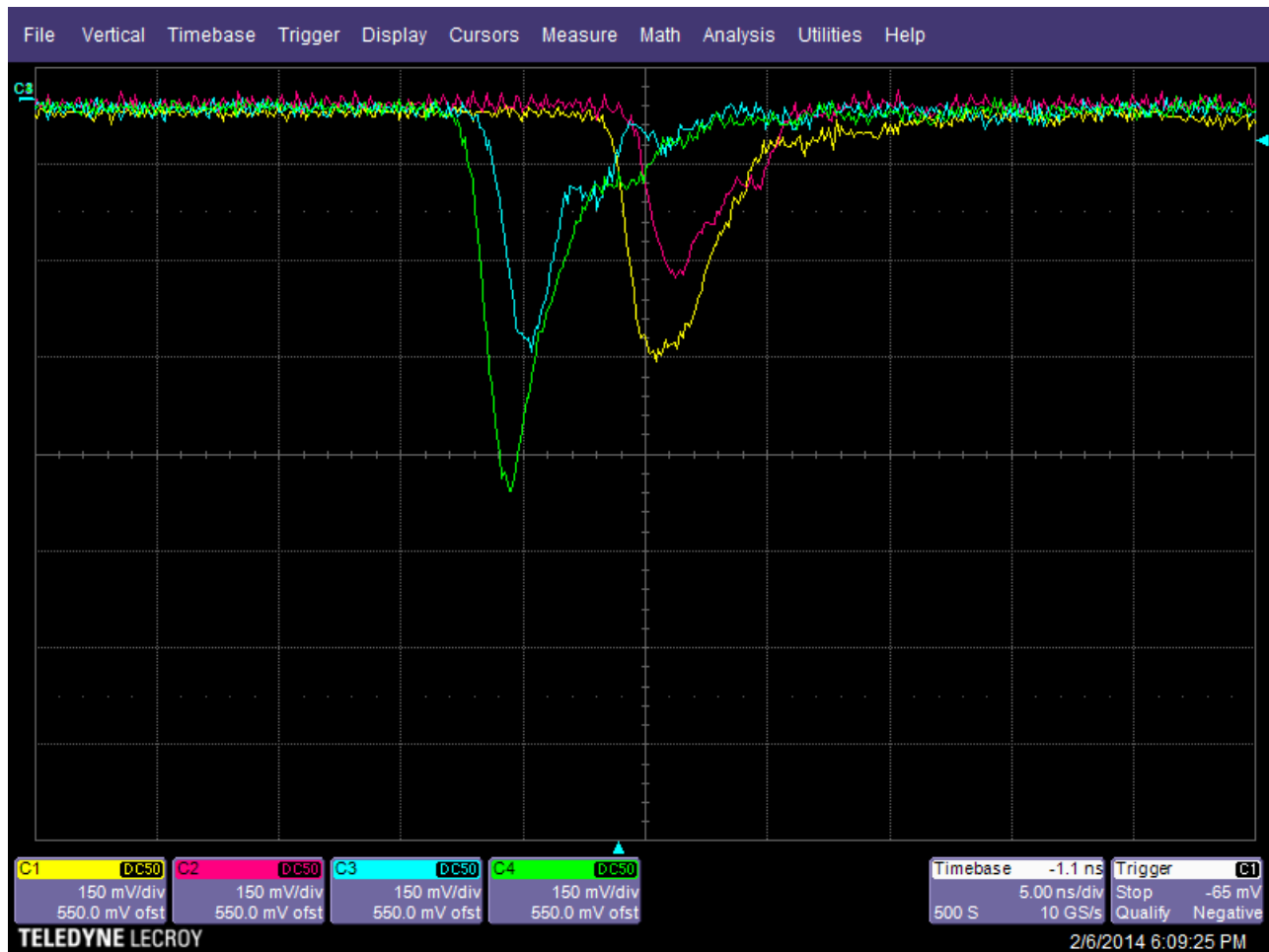
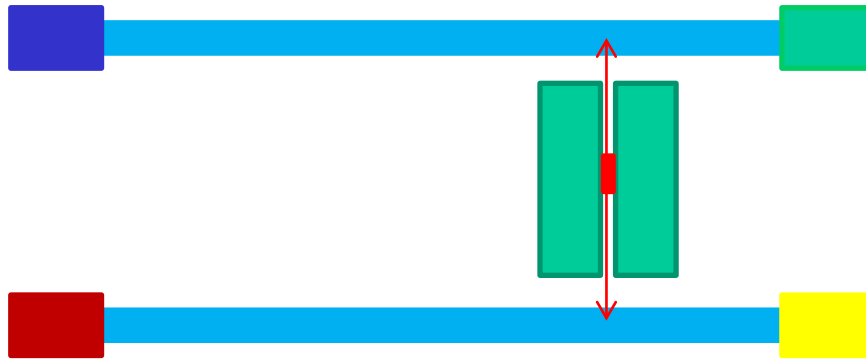


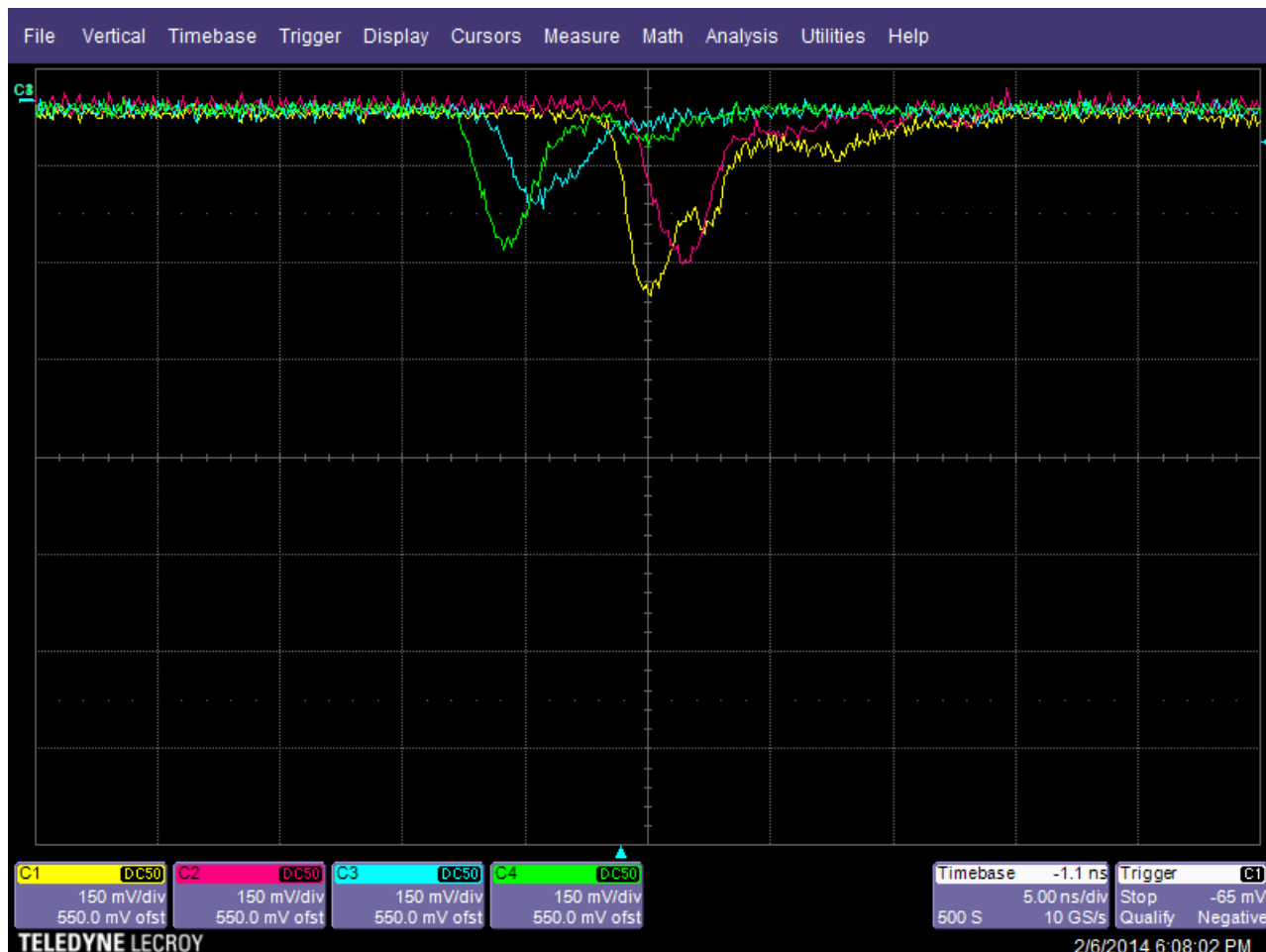
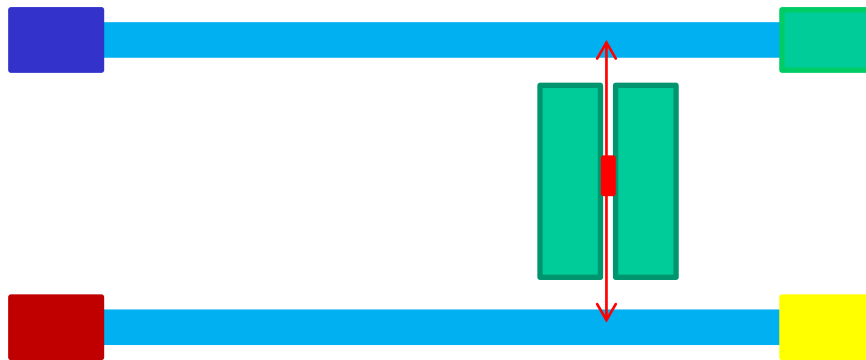








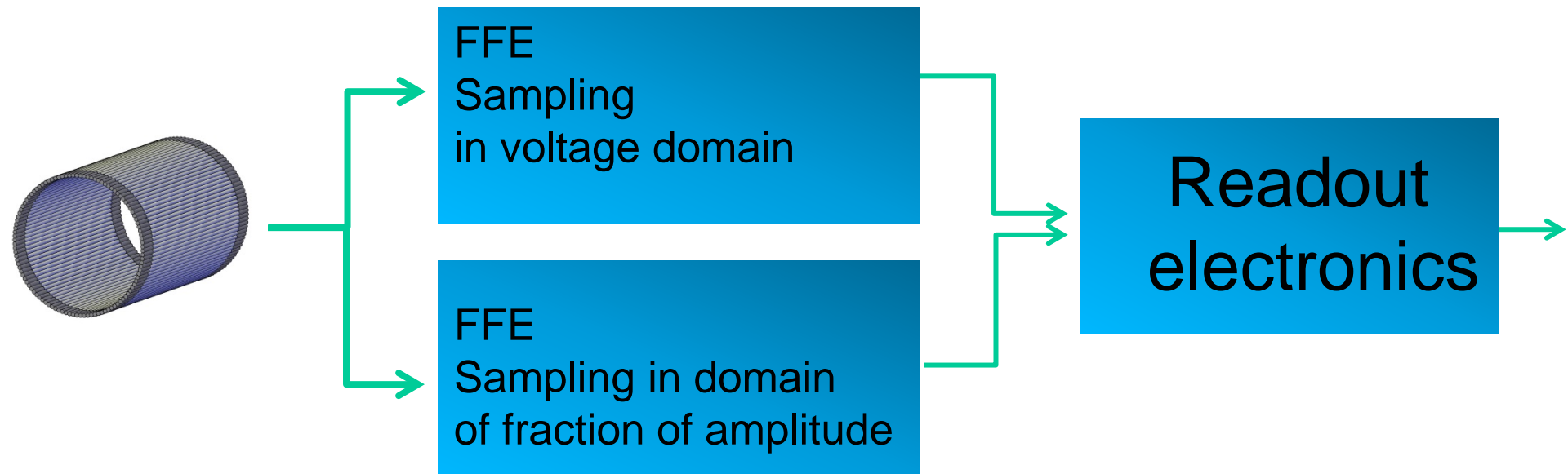


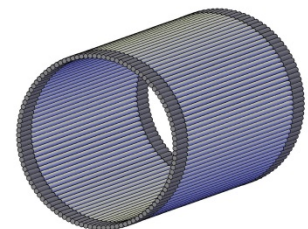


First challenge is to develop FFE electronics
with sampling precision better than 50 ps

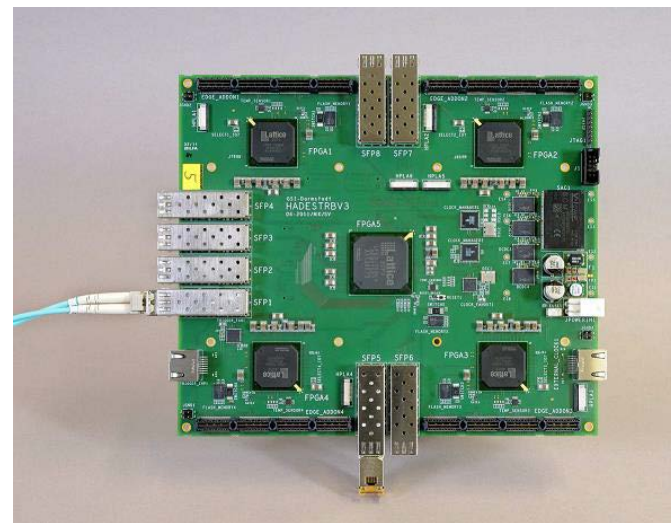
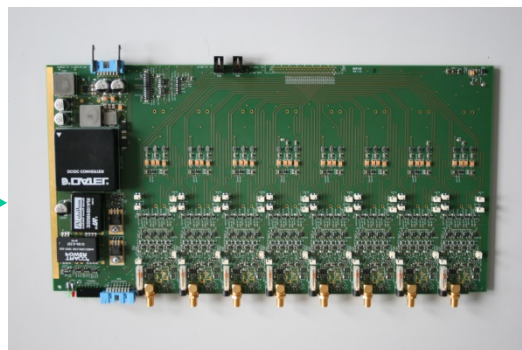
ANALOG

DIGITAL



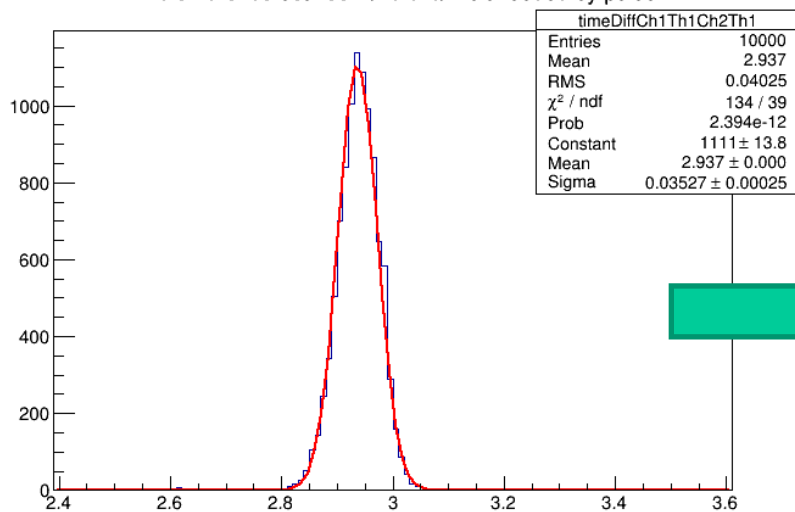


KB7 ready !



TRBv3

Time difference between two channels fed by pulser

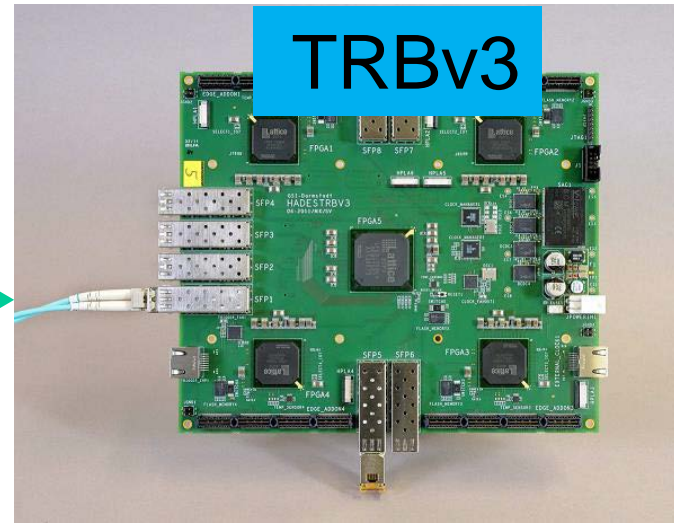


Si-Ge and As-Ge

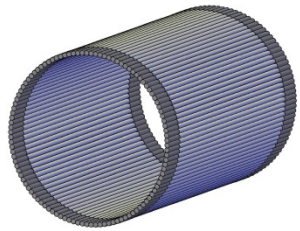
KB7 + TRBv3 together
 $\sigma(t) = 25 \text{ ps}$



KB7 ready !

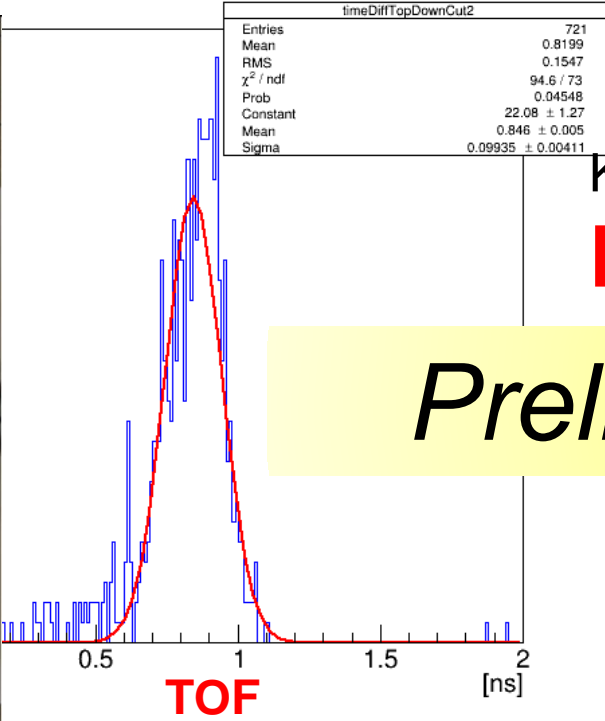
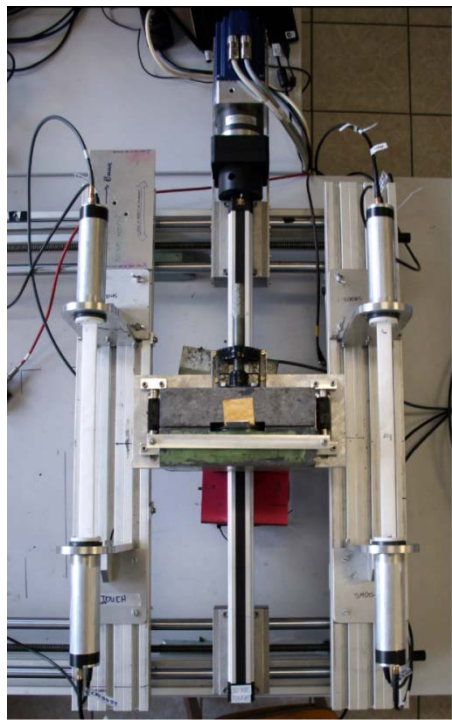


TRBv3



Triggerless mode !
PCT/EP2014/068352

Time difference between two strips after cut on TOT



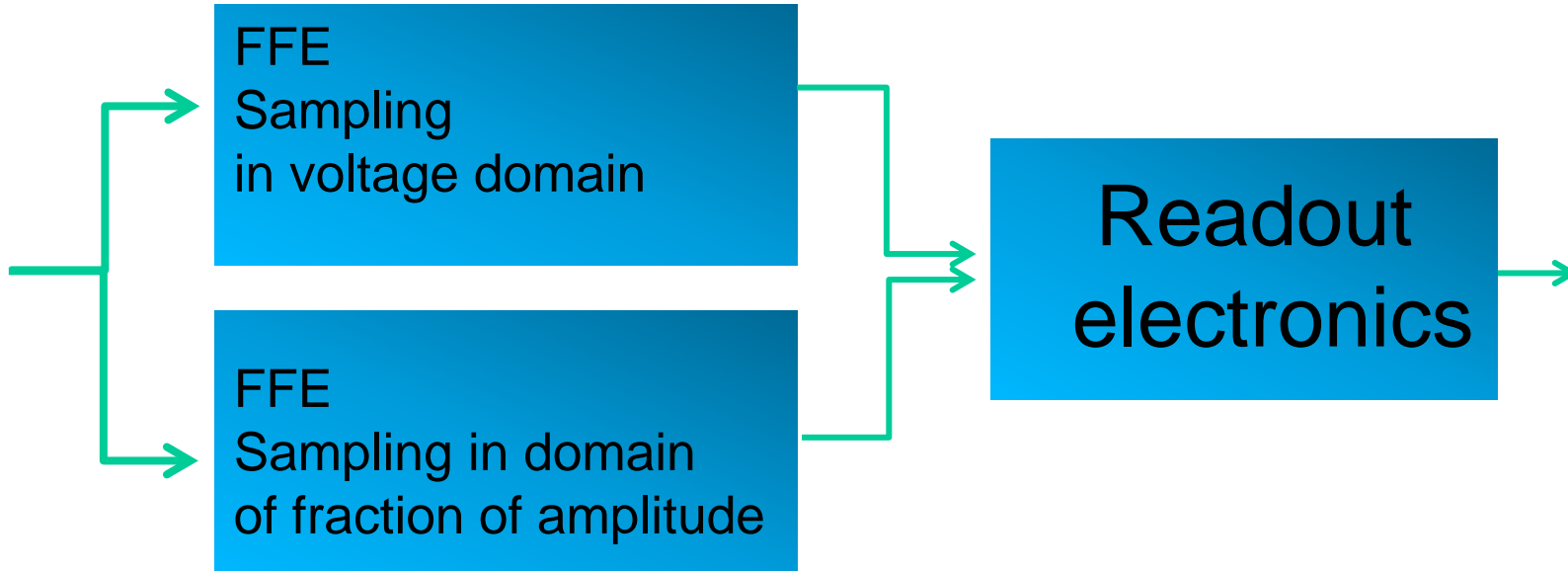
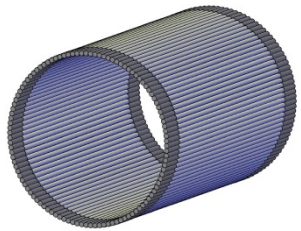
KB7 + TRBv3 with single threshold
FWHM(TOF) < 220 ps

Preliminary

Compared to ~ 600 ps
of current TOF-PET

ANALOG

DIGITAL



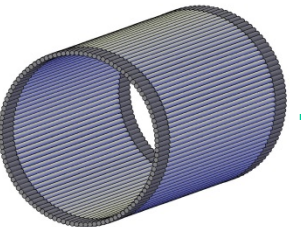
New idea... BREAK THROUGH

ONLY DIGITAL

FFE sampling & Readout electronics

PCT/EP2014/068367

precision of 21ps (sigma) for 10 Euro per sample



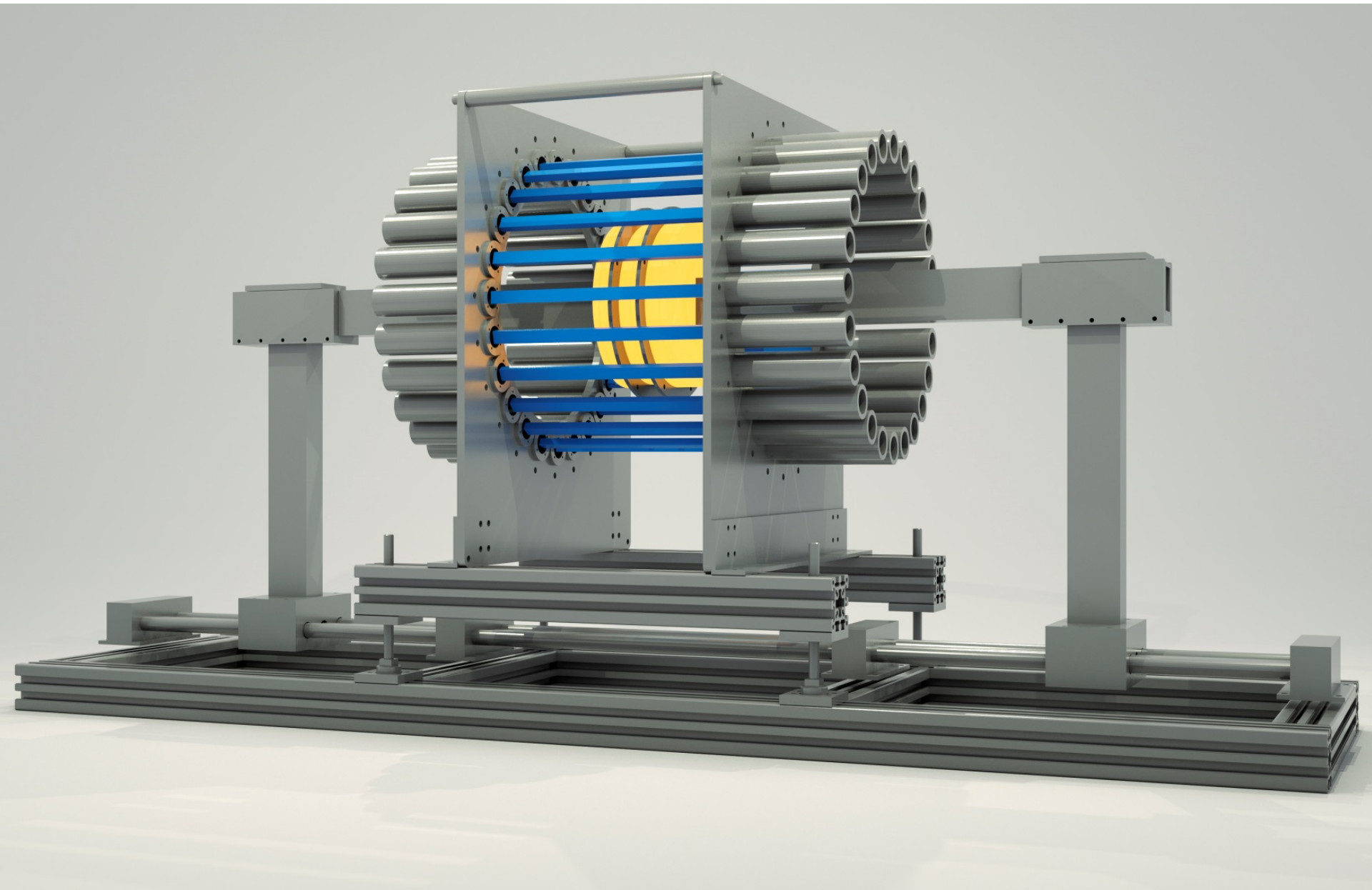
simultaneous PET-CT scan: PCT/EP2014/068363
and
simultaneous PET-MRI scan: PCT/EP2014/068373

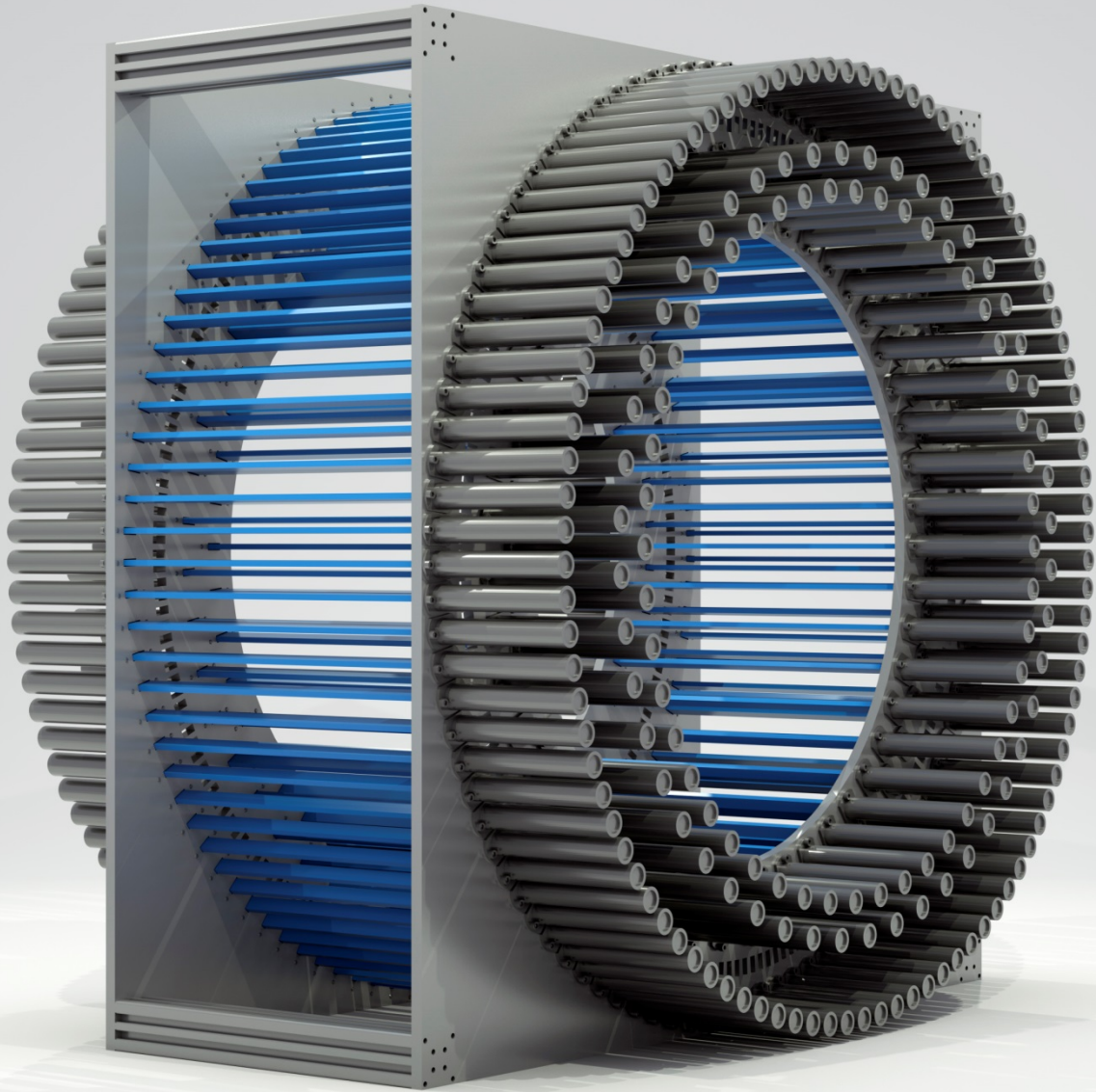


petct_animation41_loop.mp4



Z³ożenie_PET_MRI.avi







**INSTYTUT
FOTONOWY
COMPANY**



ELECTRONICS

P. Salabura, T. Kozik,
M. Pałka, P. Strzempek

**Nowoczesna Elektronika
COMPANY**



DAQ TRIGGERLESS
G. Korcyl, M. Kajetanowicz



Analysis framework
W.Krzemień, T. Gruntowski,
A.Gruntowski



**TIME and HIT-POSITION
RECONSTRUCTION**
L. Raczyński, N. Sharma, N.Zoń

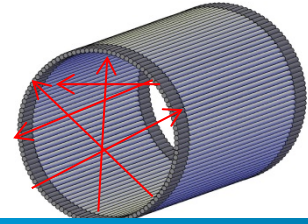


IMAGE RECONSTRUCTION
P. Białas, J. Kowal, Z. Rudy,
A. Słomski, A. Strzelecki



**IMAGE
VISUALISATION**

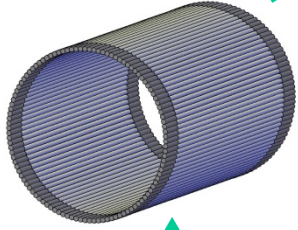
**SILVERMEDIA
IT COMPANY**

SIMULATIONS

P. Kowalski, W. Wiślicki
(Świerk Computing Centre)
D. Kamińska, O. Rundel

EXPERIMENTS, CALIBRATIONS

D. Alfs, T. Bednarski, E. Czerwinski,
J. Smyrski, E. Kubicz,
Sz. Niedźwiecki, M. Silarski,
M. Zieliński



**SYNTHESIS OF
SCINTILLATORS**

Ł. Kapłon,
A. Wieczorek,
A. Kochanowski,
M. Molenda,
A. Danel (AU)



**THANK YOU
FOR YOUR ATTENTION**